

Development of the Fast and Efficient Gamma Detector Using Cherenkov Light for TOF-PET

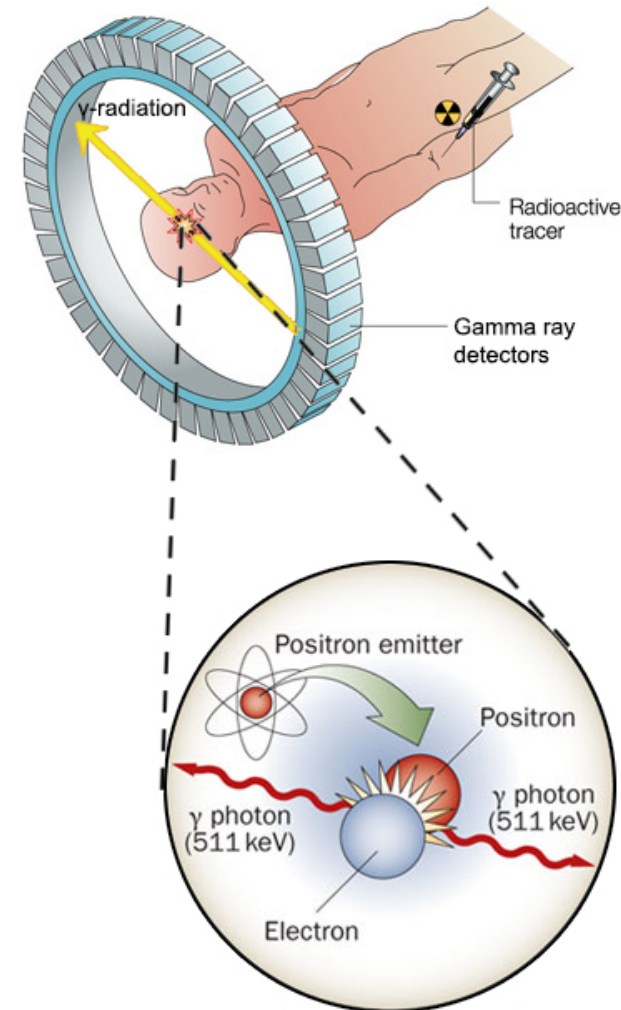
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- Functional 3-D imaging technique in nuclear medicine
 - **Oncology** : small tumors and metastases imaging
 - **Neurology** : exams of neurodegenerative diseases (Alzheimer, Parkinson)
 - ...
- **Principle** :
 - ✓ **Radioactive tracer** (ex : FDG) is injected in the patient body and then chemically bounded in tissue
 - ✓ **β^+ decay** : emission of a **positron**
 - ✓ **Annihilation** with an electron of tissue : **two 511 keV γ** are emitted back-to-back
 - ✓ Detection in **coincidence**
 - ✓ **Image reconstruction**
- Important characteristics of PET detector
 - **Efficiency**
 - **Time resolution**
 - **Spatial resolution**



Provides information on the localisation of the annihilation vertex on the Line-Of-Response (LOR).

Goal : achieve time resolution of 100 ps (FWHM)

→ localisation of 3 cm on the LOR

→ Improvement of the image signal-to-noise ratio

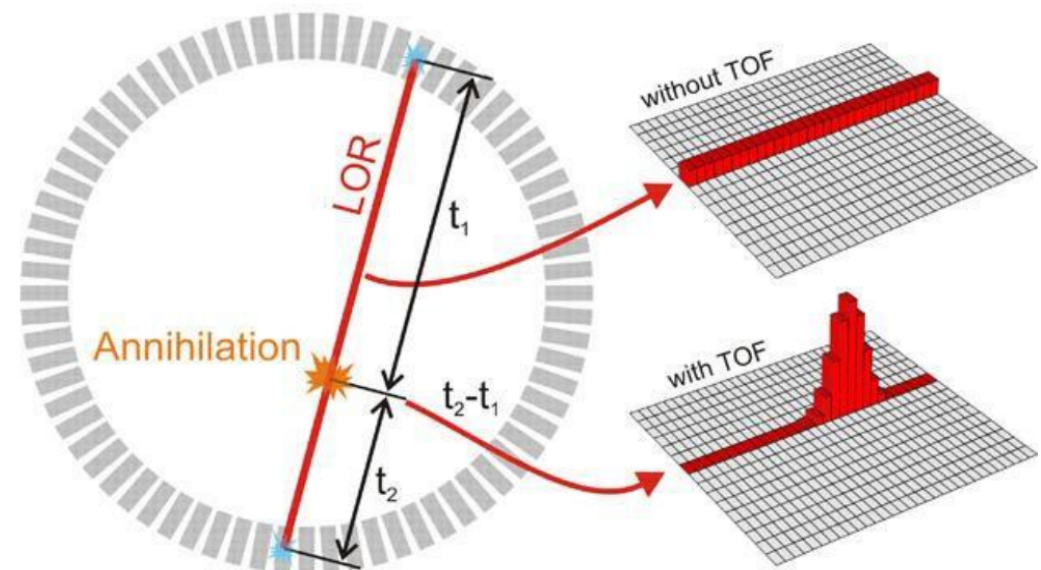
$$\text{gain} = \sqrt{\frac{2 \cdot D}{c \cdot \delta t}}$$

For example,

With * $D = 20 \text{ cm}$ (organ size)

* $\delta t = 100 \text{ ps}$,

gain in contrast is 3.6



Improvement of the **signal-to-noise ratio** :

- **reducing of the radiation dose** received by the patient while keeping the same image quality,
- or, alternatively, **improvement of the image quality** without increasing the received dose.

Current PET-scan uses **scintillation**

~ **10 to 50 ns**

To improve the TOF : using of **Cherenkov radiation**

fast : ~ 10 ps

but low yield

→ **development of 2 twin projects : CaLIPSO and PECHE**

→ Construct a Cherenkov detector
with high detection efficiency and time resolution

→ **PbF₂ crystal (10 mm) :**

- * very fast with Cherenkov radiation
- * one of the highest photoelectric fraction : 46 %
- * optical refractive index : 1.82 for $\lambda=400$ nm
- * near perfect optical transparency between 250 nm and infrared wavelengths
- * large density : 7.66 g/cm³

→ **Optical gel (OCF 452) :**

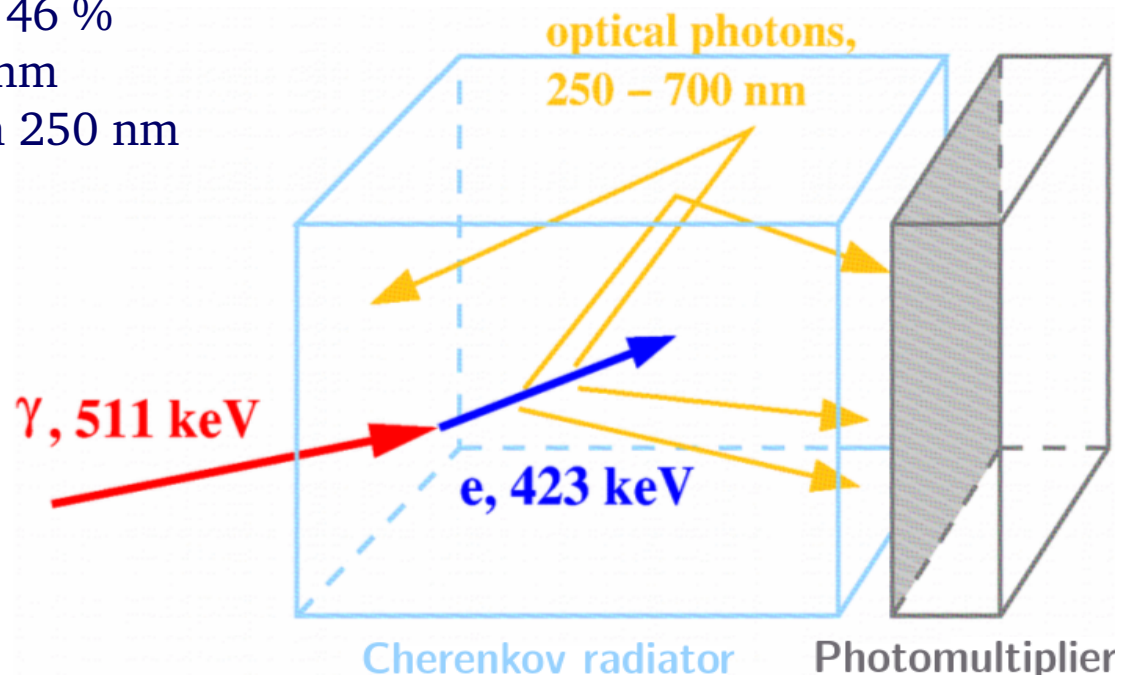
- * refractive index : 1,55 (400 nm)
- * transparent up to 300 nm

→ **MicroChannel Plate-PMT (Photonis)**

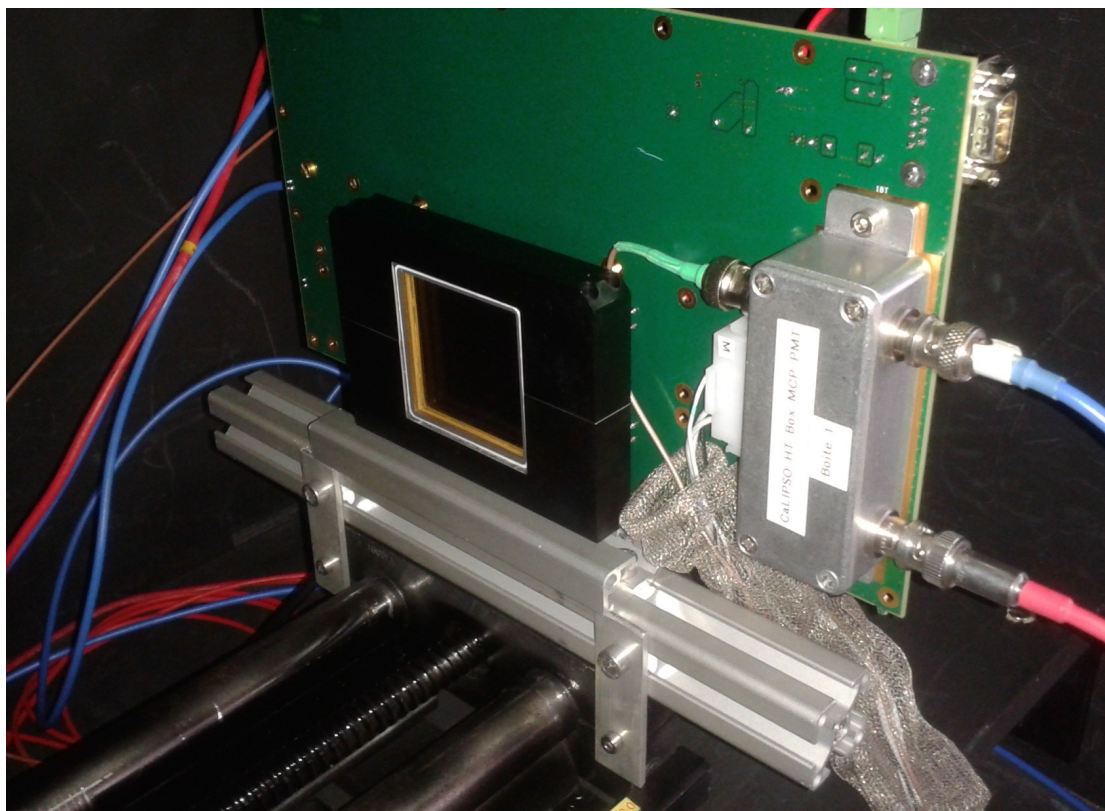
→ **Preamplifiers 2.5 GHz bandwidth, 30 dB, ZKL-2R5+**

→ **SAMPIC module : Time and Waveform Digital Converter (TWDC) chip**

KORPAR, S. et al., NIM A, vol. 654, 2011
KORPAR, S. et al., NIM A, vol. 732, 2013



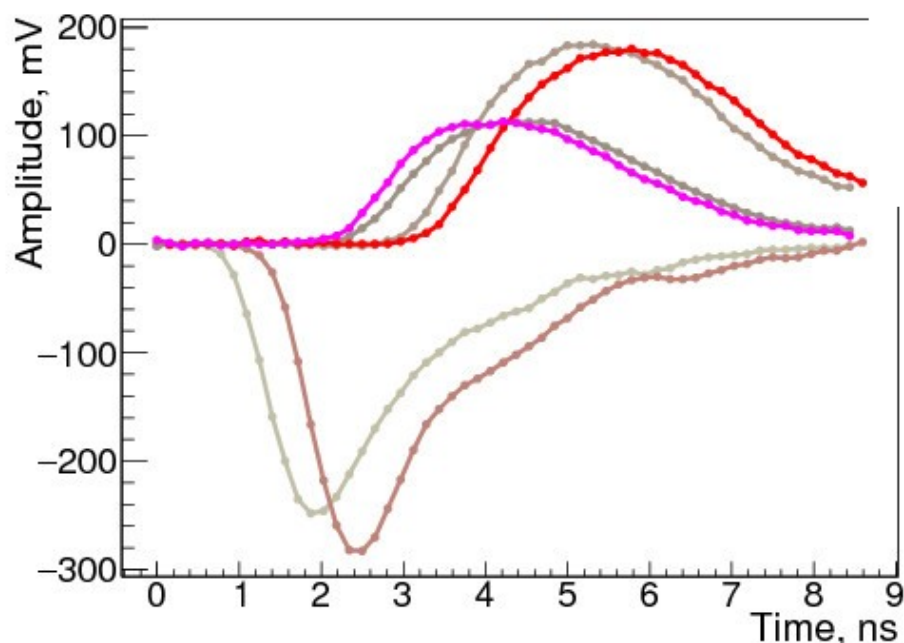
MCP-PMT Photonis *XP85012 Planacon*



- * **Low Dark Count Rate**
 $\approx 100 \text{ Hz/cm}^2$
- * **Fast :**
TTS $\lesssim 100 \text{ ps}$ (FWHM)
- * **Good quantum efficiency**
up to 25 %
- * Active surface 53 mm x 53 mm
- * Windows material : sapphire
- * 8 x 8 anodes
- * 25 μm pore diameter

Signals numerisation with the **SAMPIC** module:

A 32-channel, 10-GSPS Time and Waveform Digital Converter module, developed by IRFU and LAL.

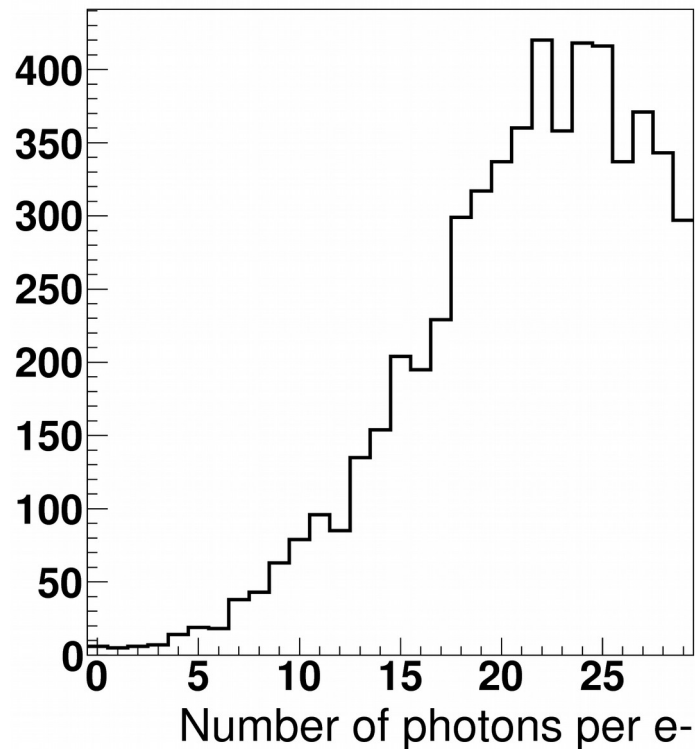
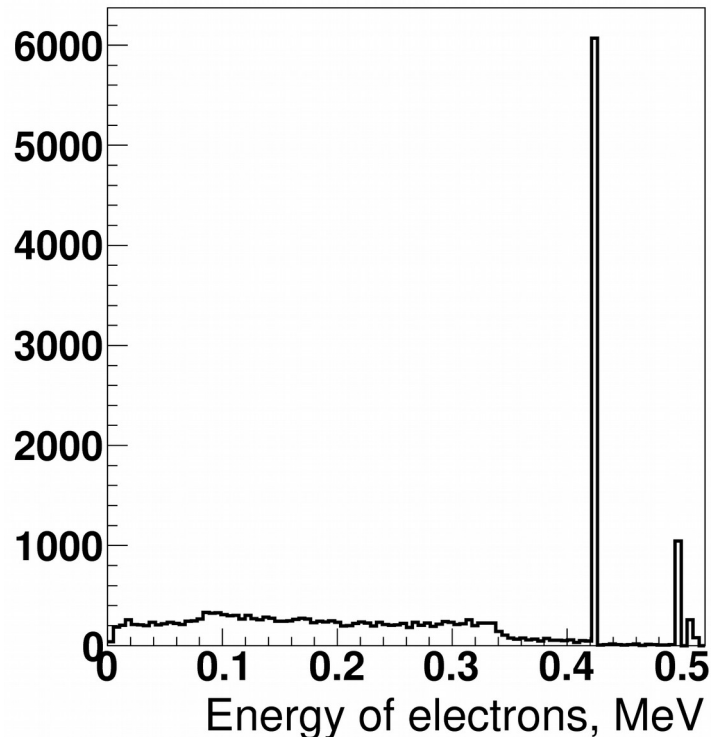


Typical signal with 6.4 GS/s

- * provides digitized waveform with 64 samples, 1.6 GS/s to 10 GS/s
- * extremely good resolution in time : $< 5 \text{ ps } (\sigma)$
- * allows to use on-line the configurable Constant Fraction Discriminator (CFD) algorithms
- * acquisition of waveform and/or CFD time

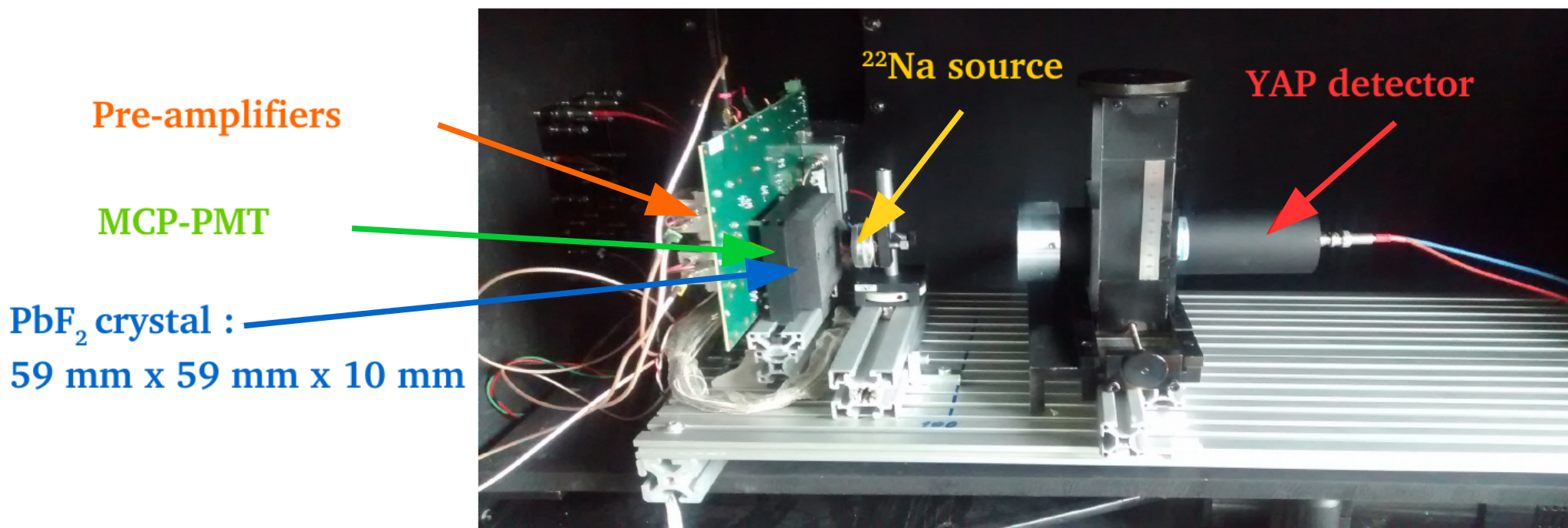
→ A 511 keV gamma enters the crystal,
what probability do I have to detect it ?

- * gamma-conversion efficiency : 67 % for 10 mm crystal
- * photoelectric conversion in PbF_2 : 46 %
- * optical coupling from crystal to PMT
- * quantum efficiency of photocathode : up to 25 %



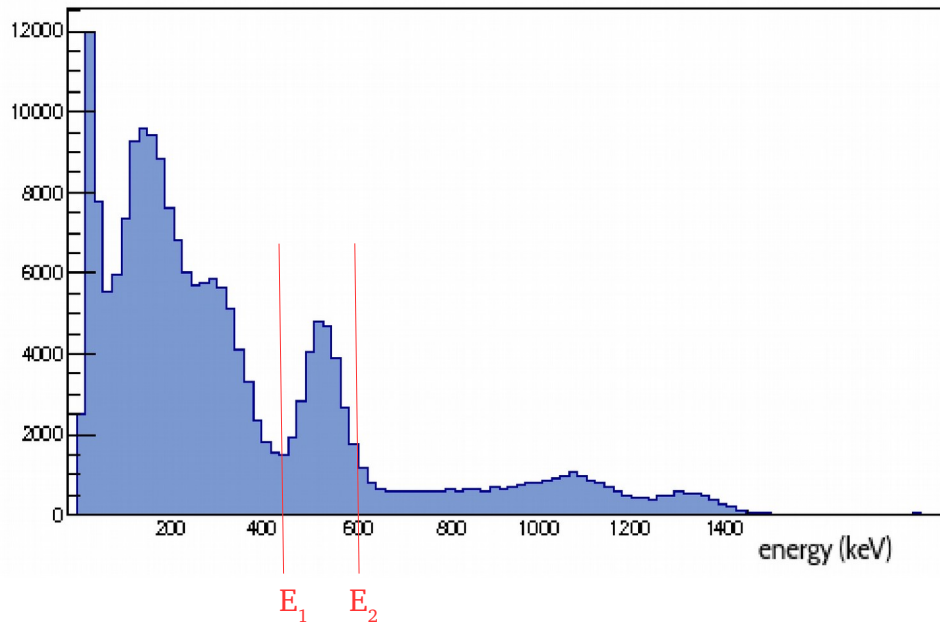
Simulation gives
an efficiency of
about 30 %

→ Measured with reference YAP detector with « Tag & Probe » method



- In order to know when a 511 keV gamma entered on the detector
- selection of the 511 keV events in the YAP
 - look at the coincidence events in the PbF₂

YAP energy spectrum



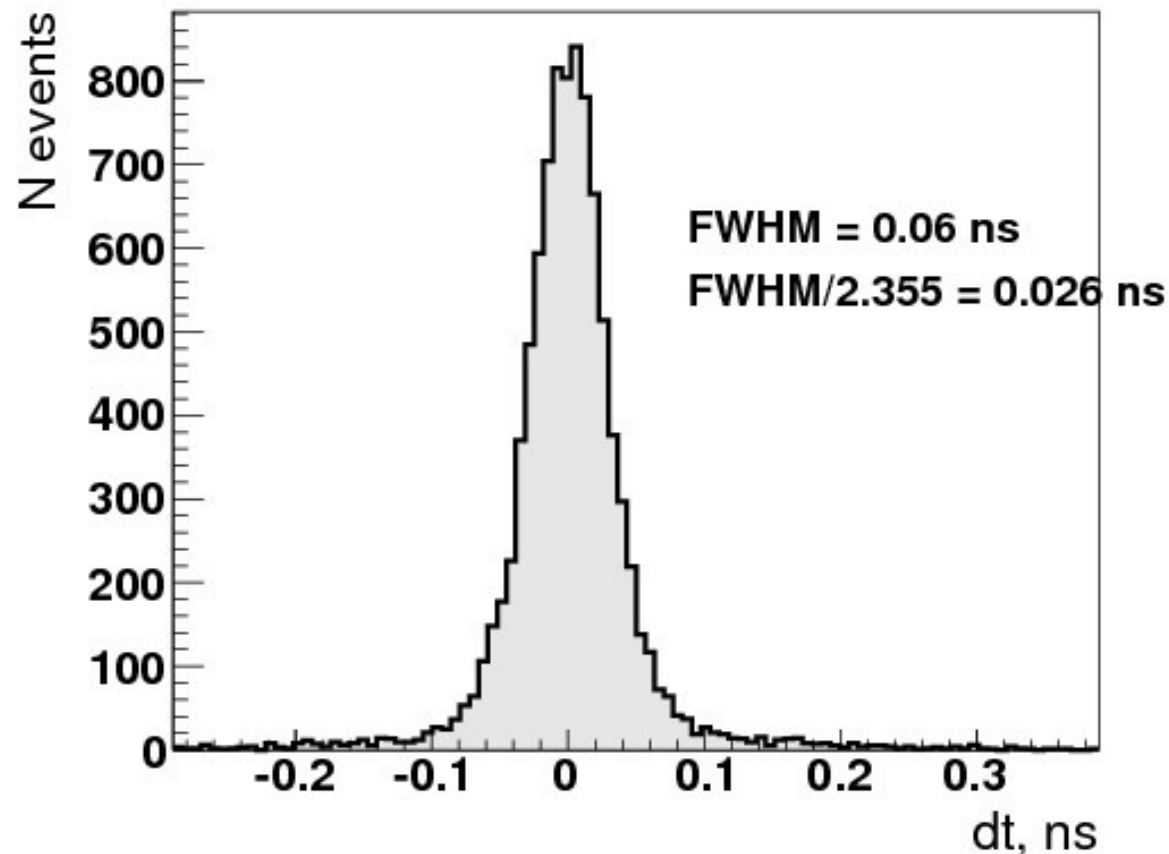
$$\text{Eff} = \frac{N(\text{PbF}_2)}{N_{\text{YAP}}(E > E_1, E < E_2)}$$

Eff ~ 28 % (*preliminary*)

Systematic effects taken into account :

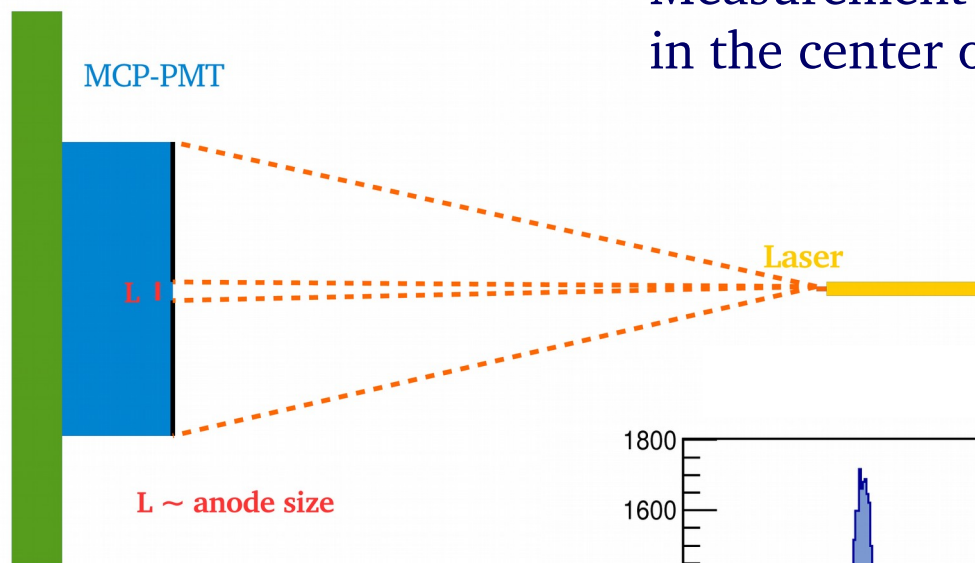
overestimation of the N_{YAP} , due to the presence of Compton scattering from 1.3 MeV Compton

Simulation of intrinsic dispersion of the optical paths in the crystal

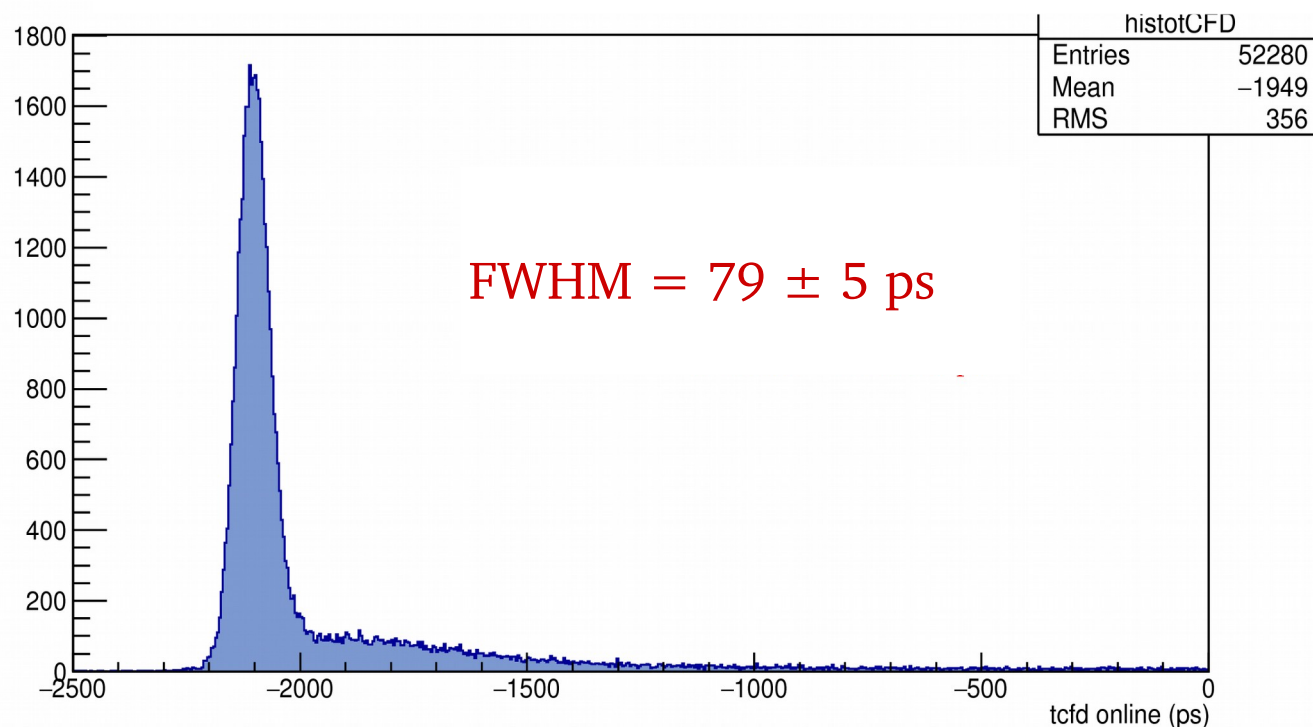


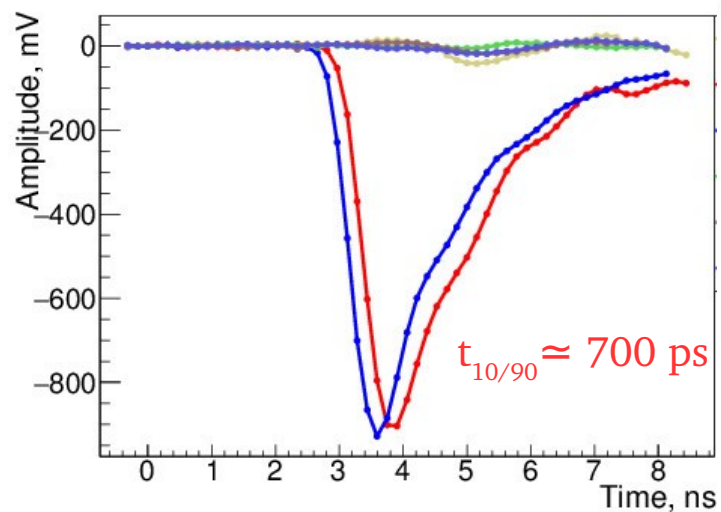
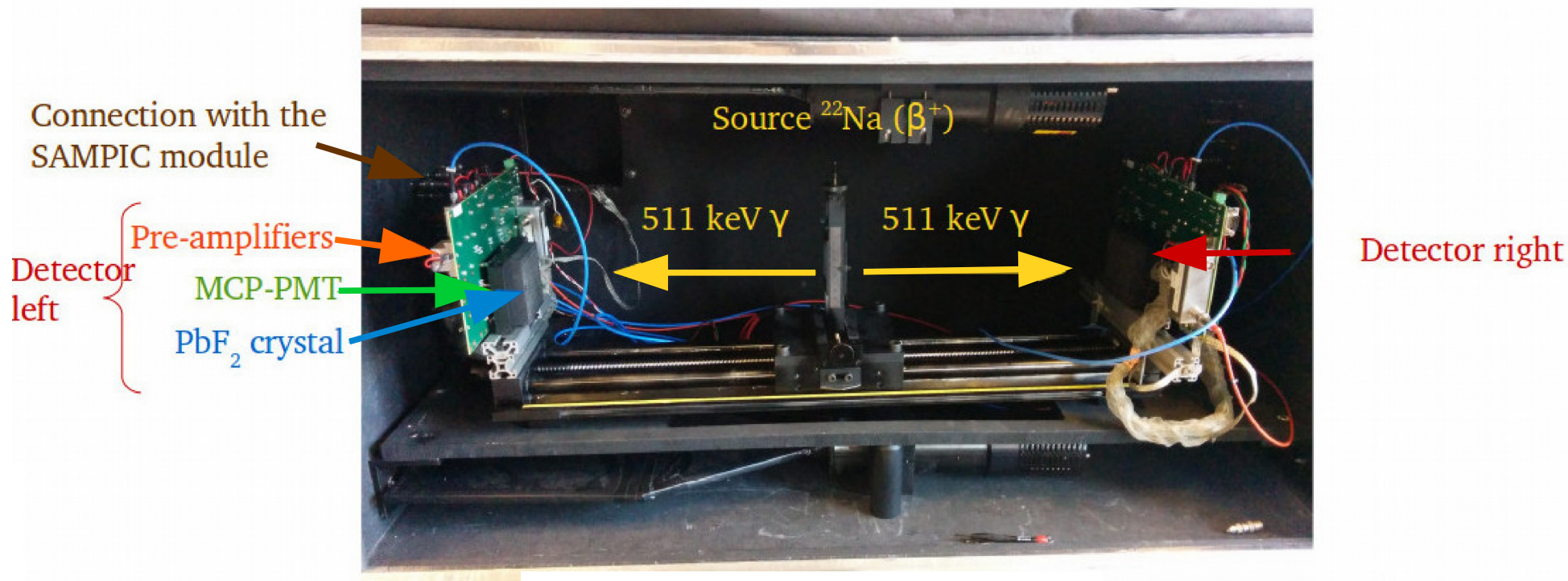
For a single detector : FWHM ~ 40 ps

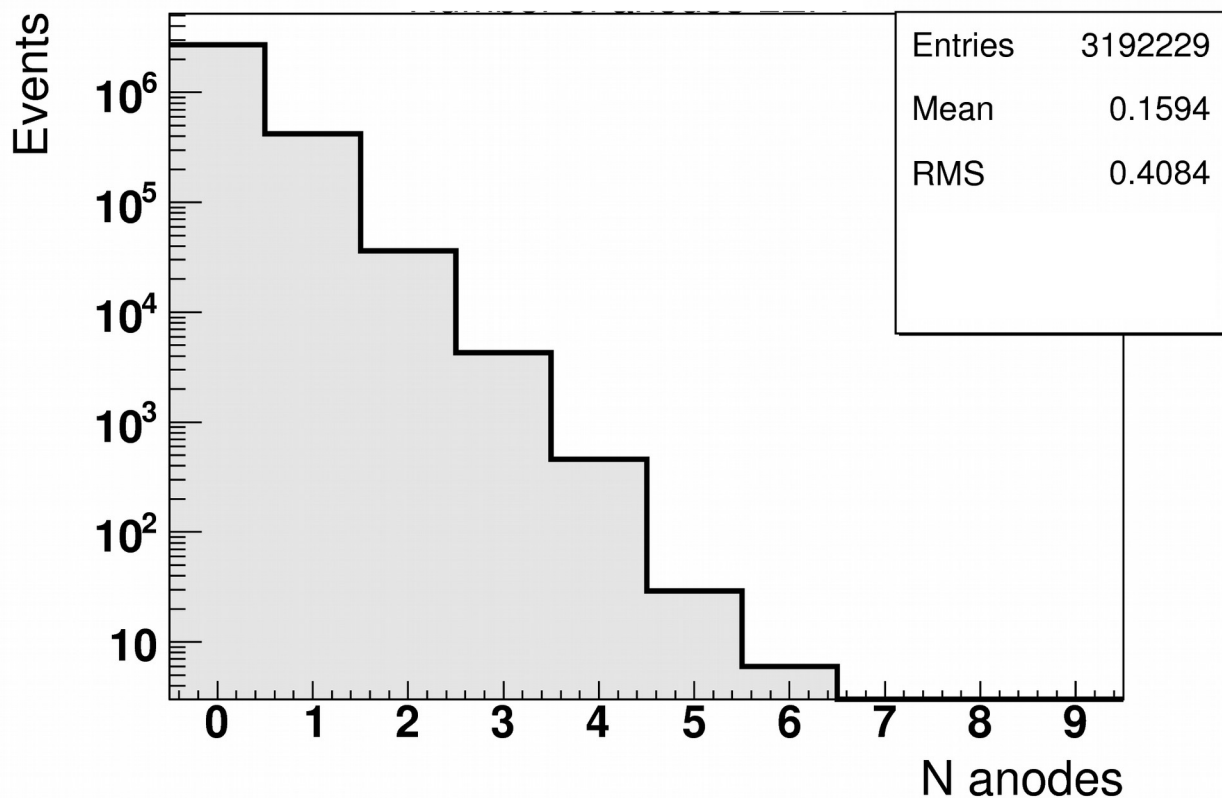
Electronic board



Measurement in a single photon mode,
in the center of MCP-PMT, laser beam width ~ 25 ps

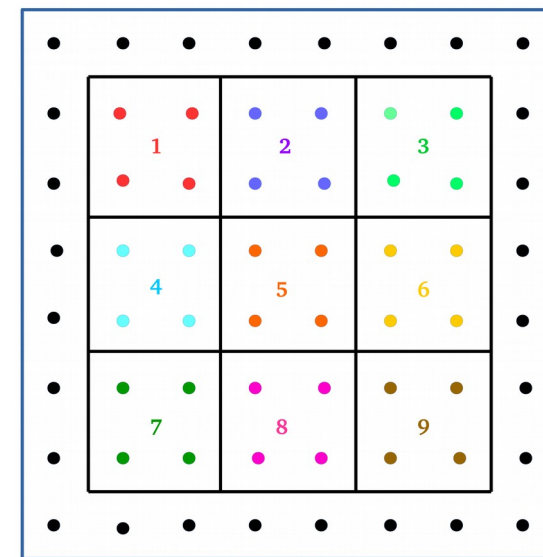




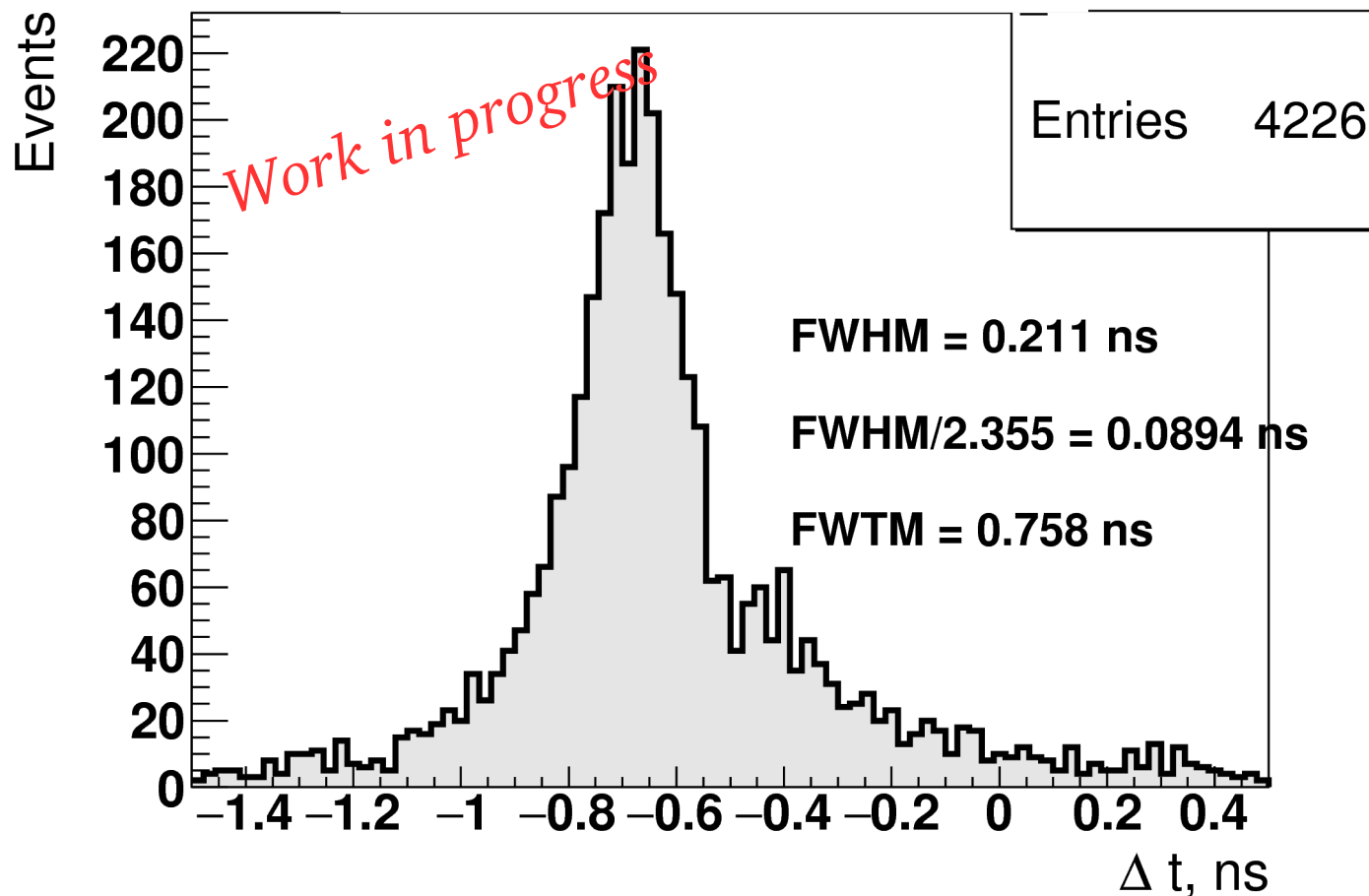


SIMULATION : Number of anode hits per PMT

- * MCP-PMT = 64 anodes
- * grouping anodes by 4
- * reading the 9 central anodes

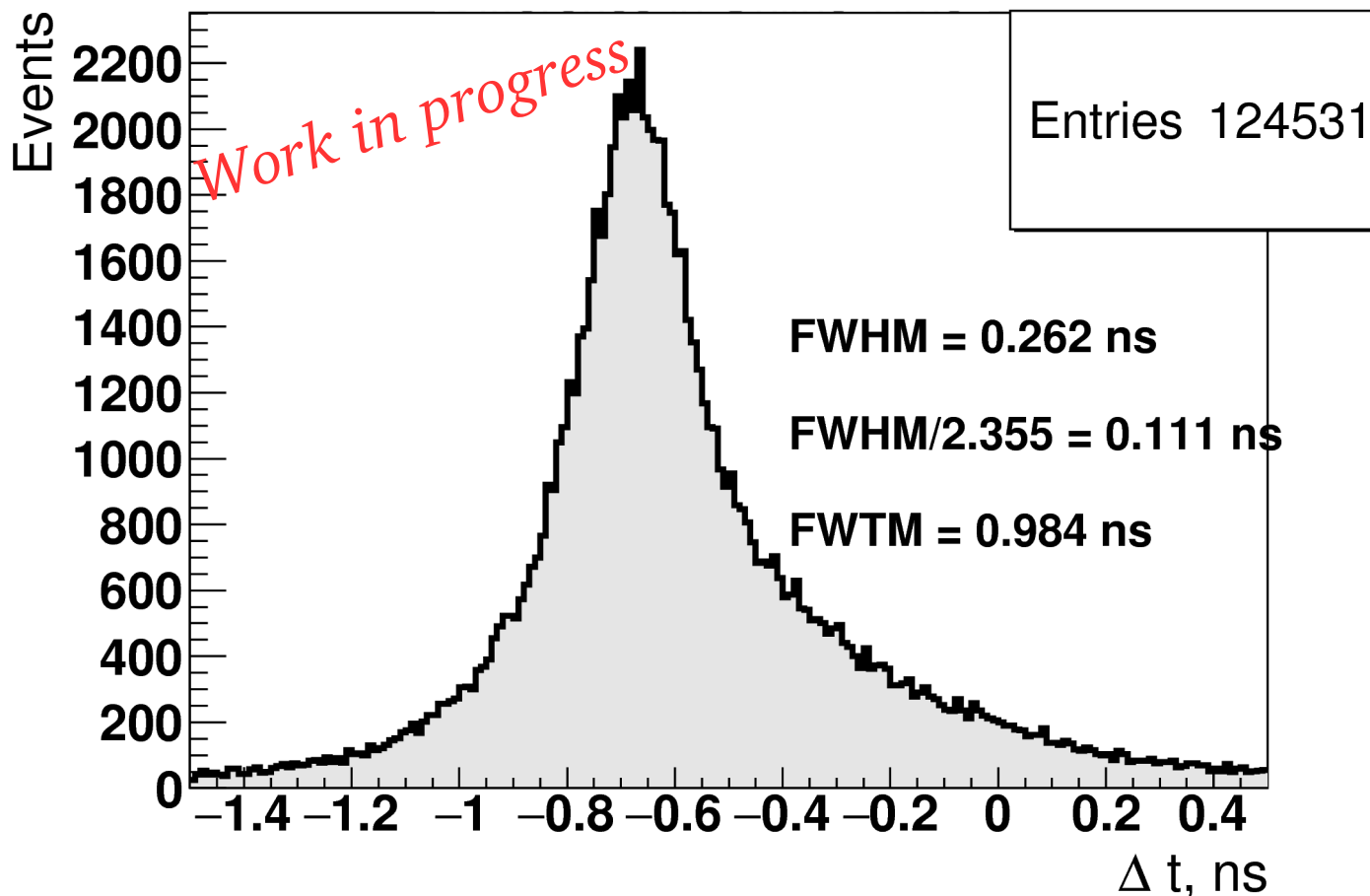


*Time Difference between the two detectors
in the MCP-PMT center*



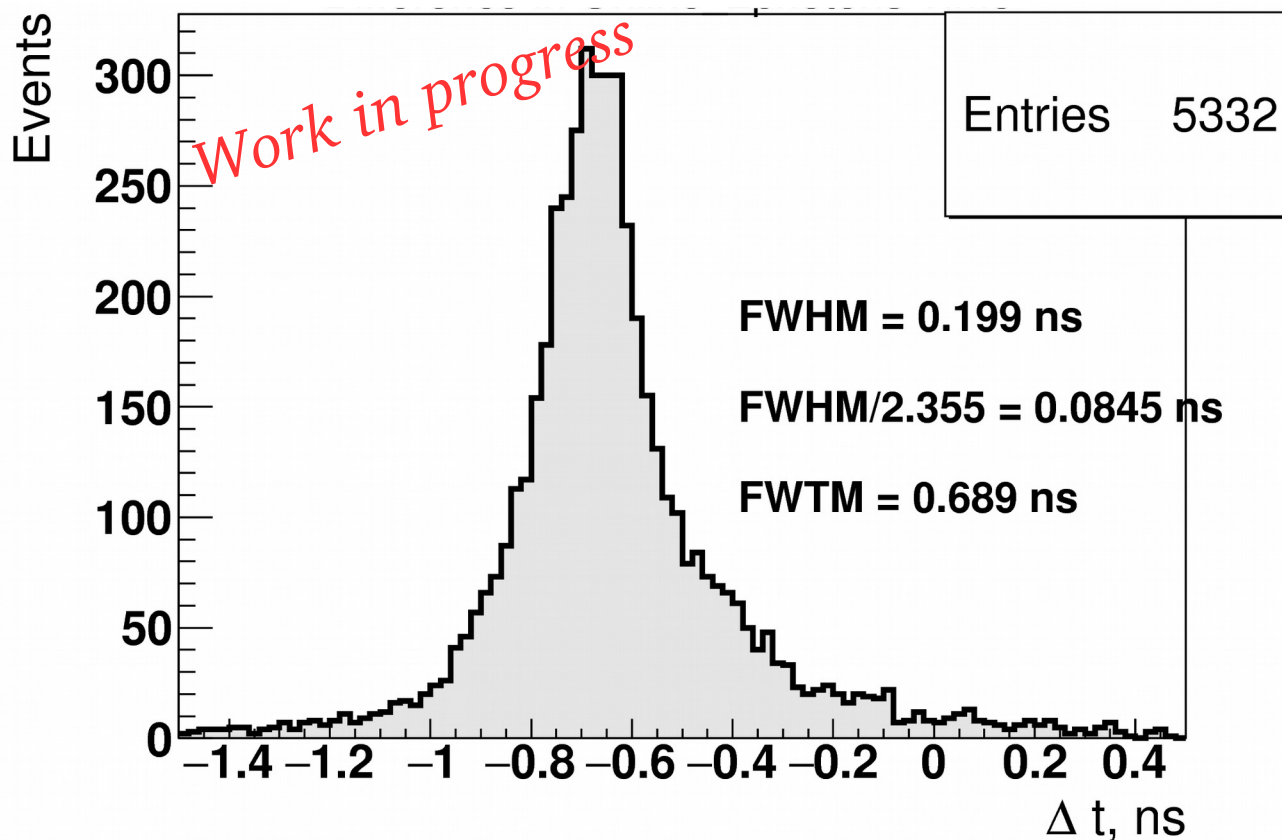
For a single detector : FWHM = (150 ± 10) ps

Time Difference between the two detectors in the full MCP-PMT



For a single detector : **FWHM = (180 ± 10) ps**

Time Difference between the detectors with a better light collection : 2 photons per MCP-PMT



For a single detector : **FWHM = (138 ± 10) ps**

→ First test with PbF_2 crystal Cherenkov detector allows us to reach an efficiency of **28 %** in rough agreement with simulations. Main degradation factor is the optical interface between crystal and windows MCP-PMT. We are working on improving it.

→ In time resolution, we measure for a single detector:

- * in the center of the detector **150 ps**.

- * in all the readable surface **180 ps**, after a first work calibration.

We are now working on the optimization on read-out electronics.

→ Twin to PECHE

→ TMBi used as liquid Cherenkov radiator

→ Previous demonstrator:

Time Resolution of (592 ± 18) ps (FWHM)

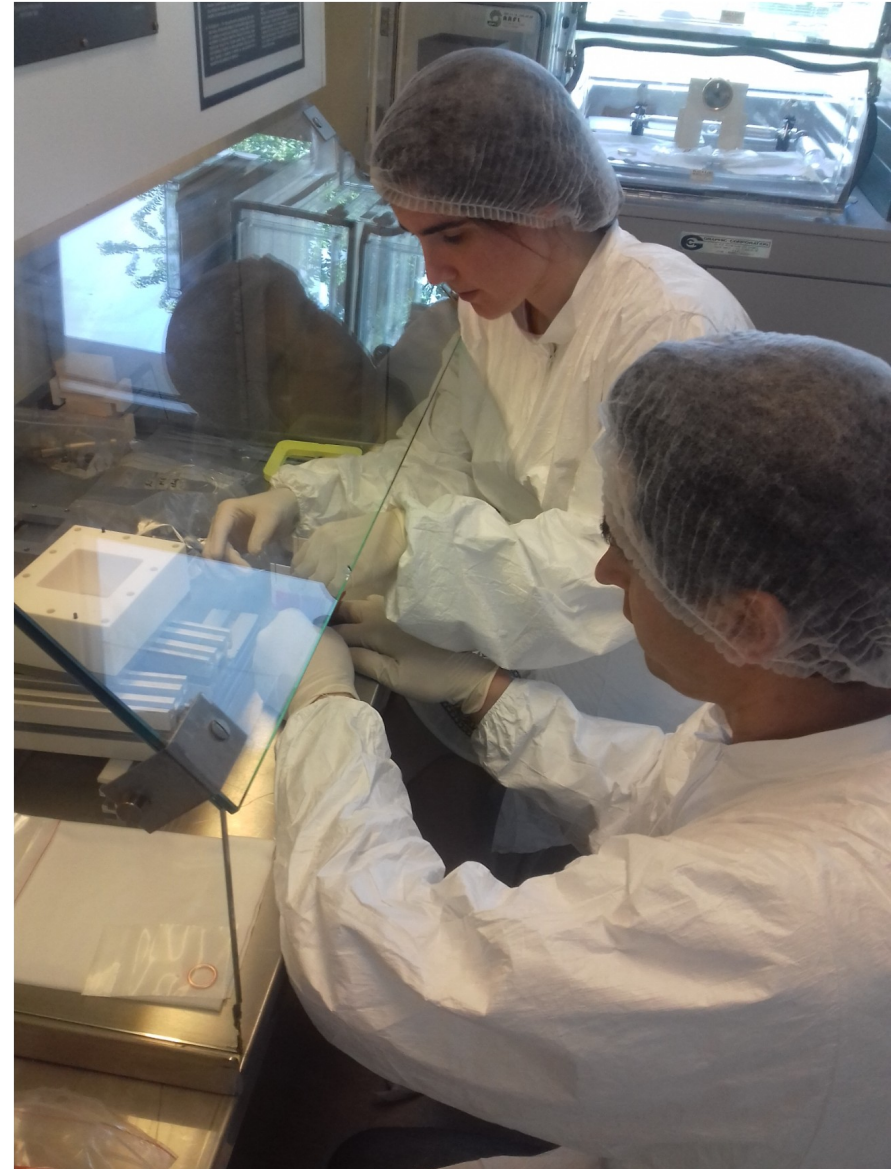
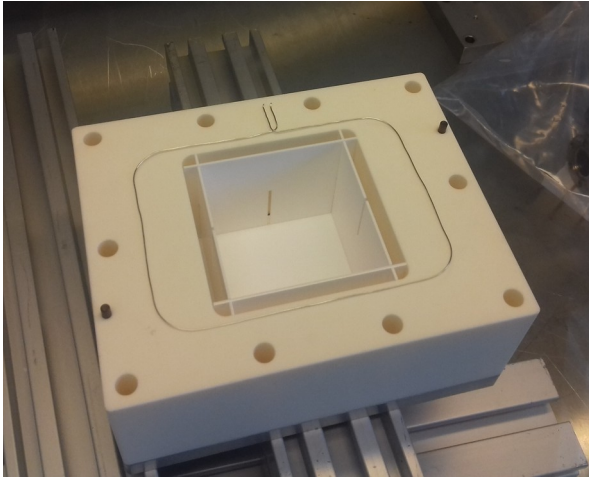
Efficiency of 34.5 %



Previous demonstrator

E. Ramos et al., « Efficient, Fast, 511-keV γ detection through Cherenkov radiation : the CaLIPSO optical detector », Vol.11 (2016) p11008

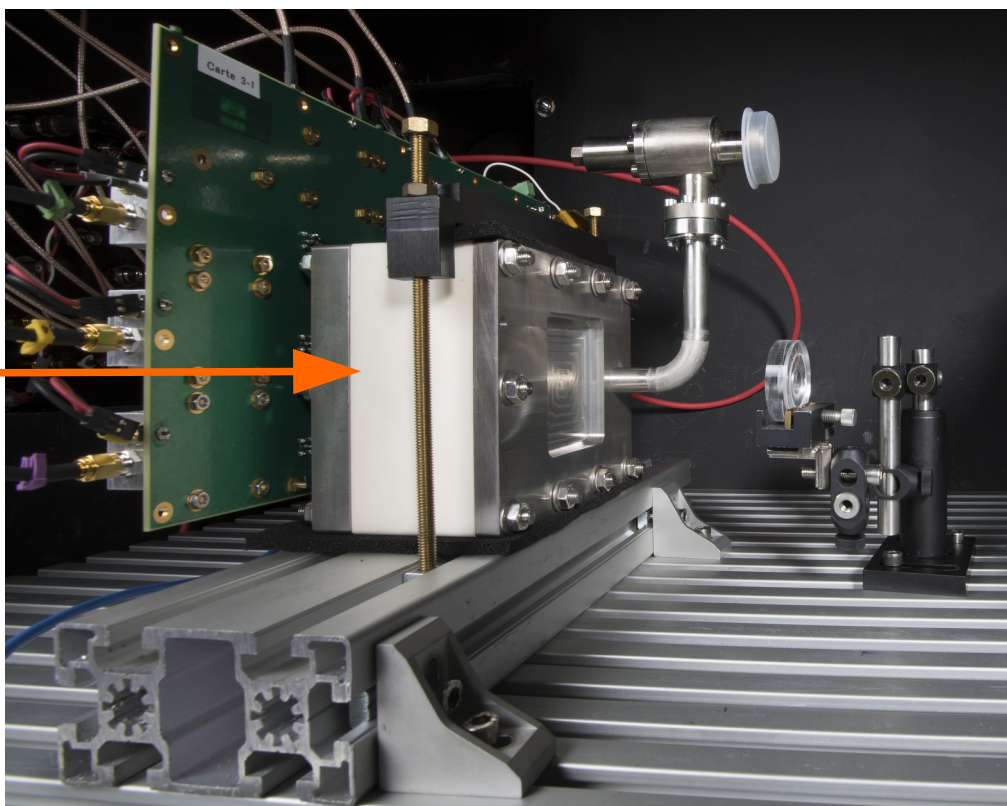
→ We now focus on **Time Resolution**, in order to reach **150 ps (FWHM)**



→ Efficiency measurement as previously : $\sim 23\%$

→ Time resolution in progress

CaLIPSO
Optical
Demonstrator



Thank you for your attention !

Back-Up

NECR = noise equivalent count rate, estimated with GATE-based simulation

