



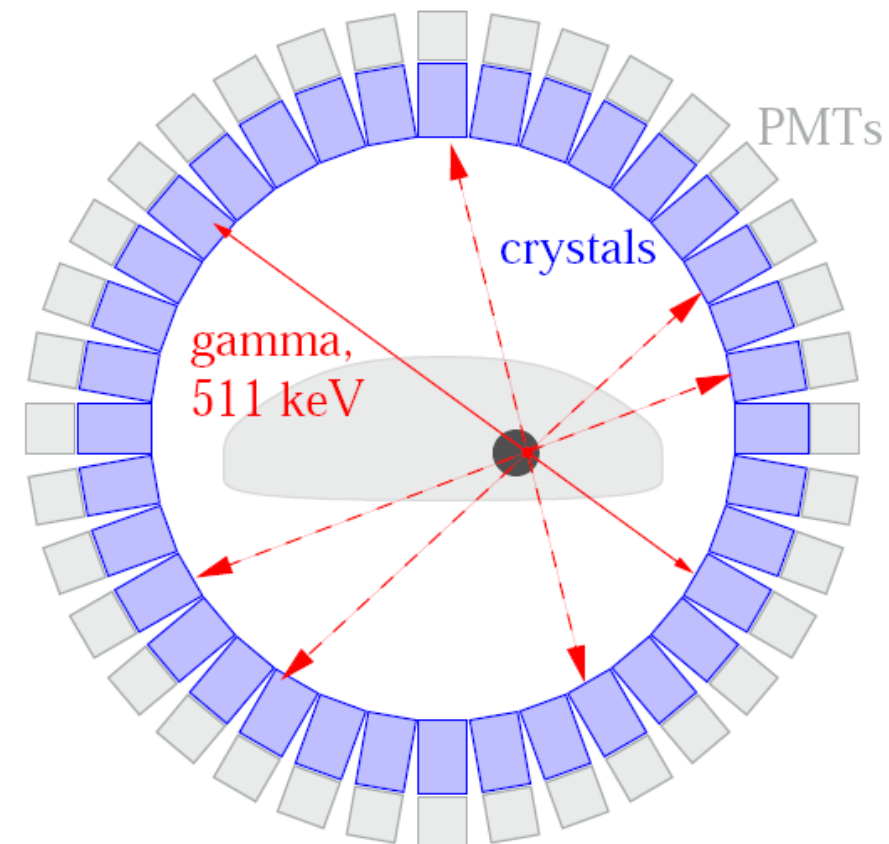
*ClearMind project: development of the  
TOF-PET detection module with tens-  
picoseconds time resolution*

*V. Sharyy  
for the ClearMind Collaboration*

French-Ukrainian Workshop on Instrumentation  
September 19, 2020

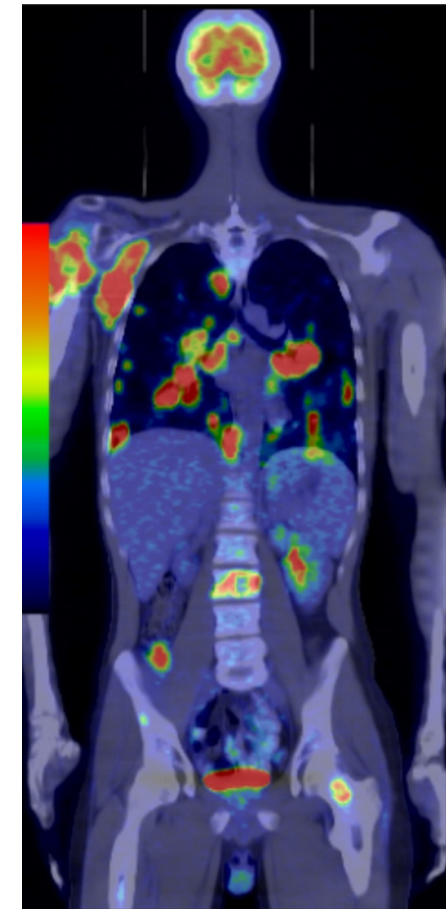
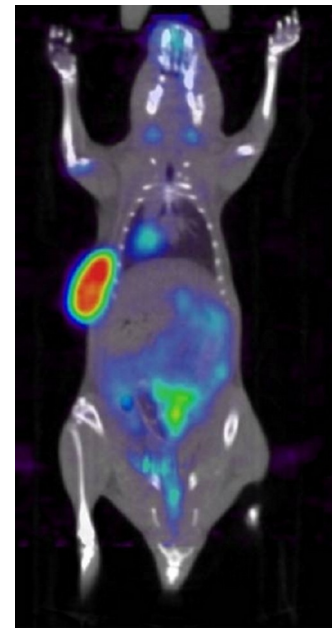
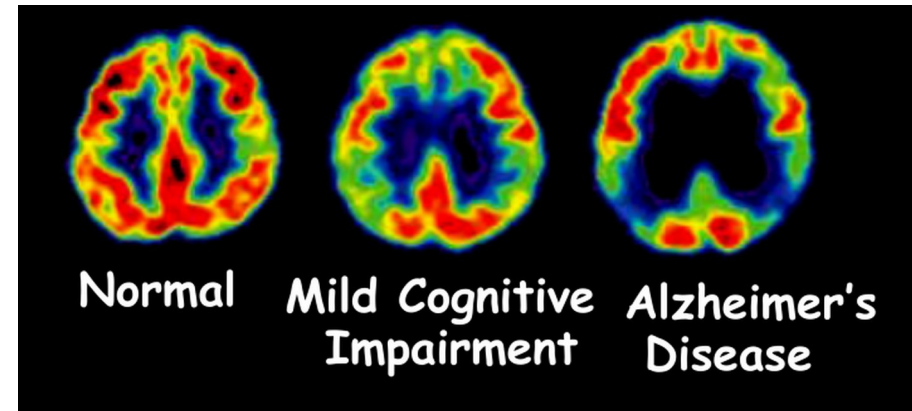
# Positron Emission Tomography

- PET is a nuclear imaging technique used widely in oncology, cardiology and neuropsychiatry.
- Allows to detect at picomol level the the biochemical activity.
- PET scan in a nootshell:
  - Inject one of the radioactive tracer e.g.  $^{18}\text{F}$ -FDG,  $\tau \sim 110$  min,  $\sim$ one hour rest time
  - emits positrons  $\Rightarrow$  annihilation with an electrons  $\Rightarrow$  two 511 back-to-back gamma.
  - Gamma detection in coincidence  $\Rightarrow$  register  $\sim 100\text{M}$  lines-of-responce  $\Rightarrow$
  - 3D image reconstruction



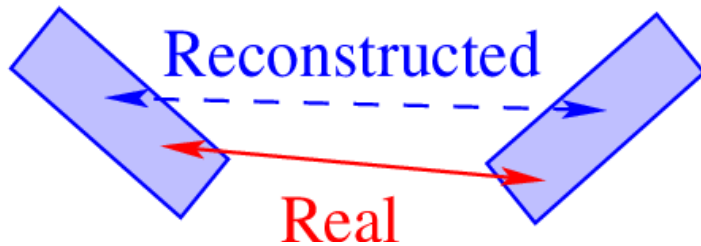
# Scanner Types

- Preclinical (small animals)
  - Small aperture
  - High spatial resolution
  - Small sensitivity
- Brain scanner
  - Limited aperture
  - High sensitivity
  - Good spatial resolution
- Whole-body
  - Large aperture
  - High sensitivity
  - Low spatial resolution
  - Full body dose ~ **5 - 15 mSv**  
(natural radioactivity per year France : 2 mSv)

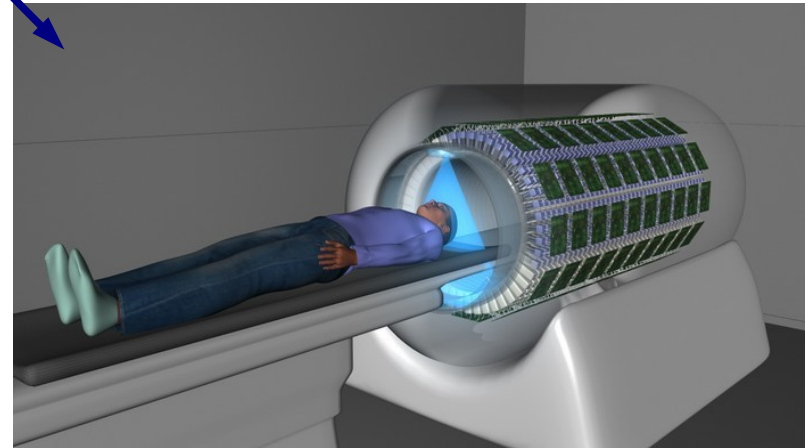
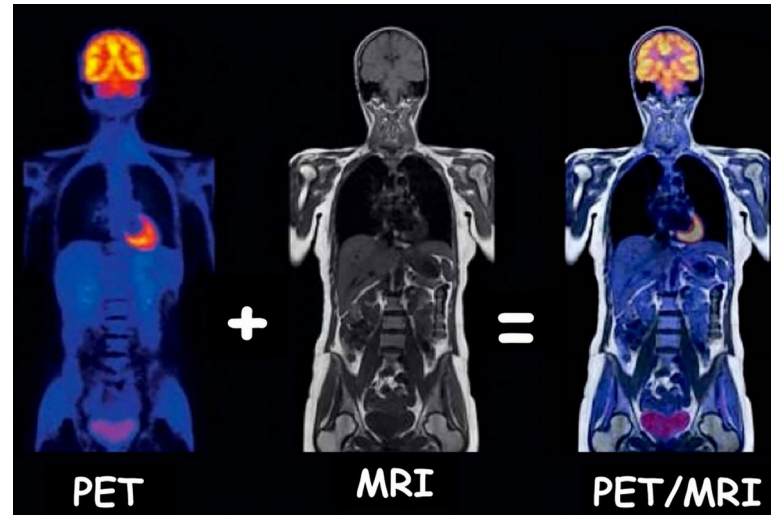


# PET Evolution

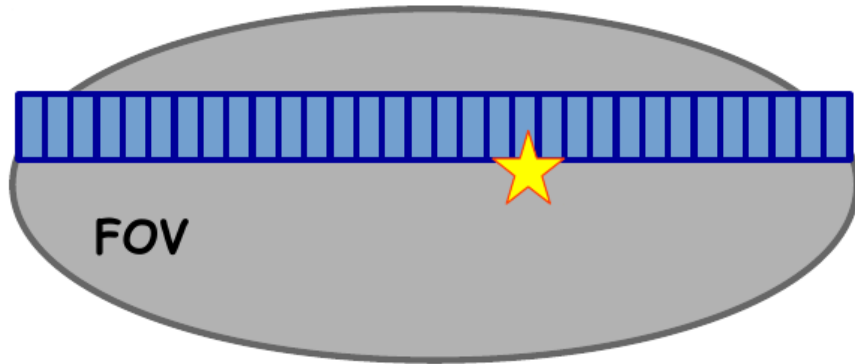
- Combined modalities: CT/PET, MRI/PET
- Improvement sensitivity: total-body PET → 40 fold improvement in sensitivity
- *Reduce bias: depth-of-interaction reconstruction*



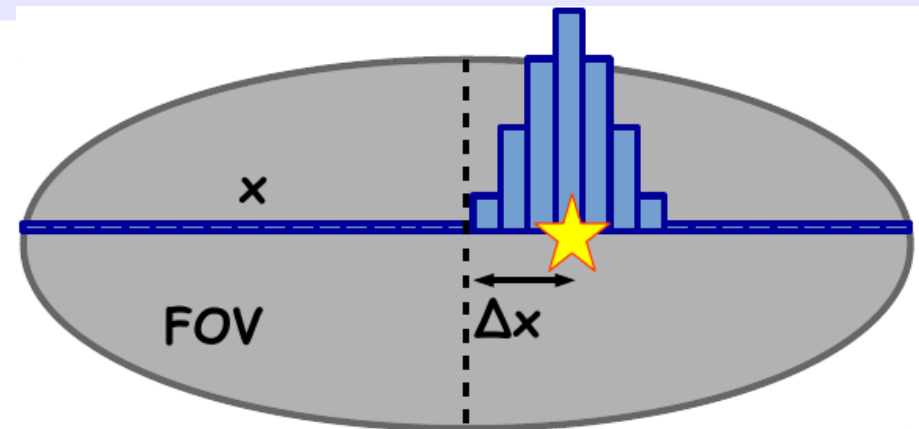
- Time-of-flight technique (TOF) ⇒ see next slides
- New developments in electronics, and gamma-detection



# TOF Technique



Conventional PET



TOF PET

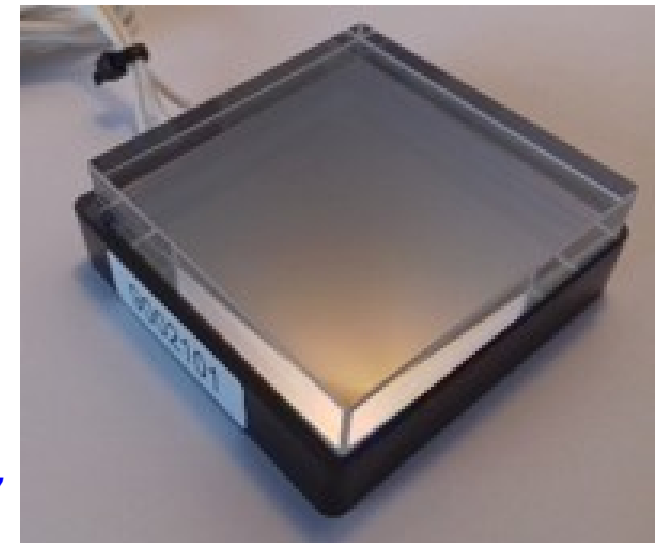
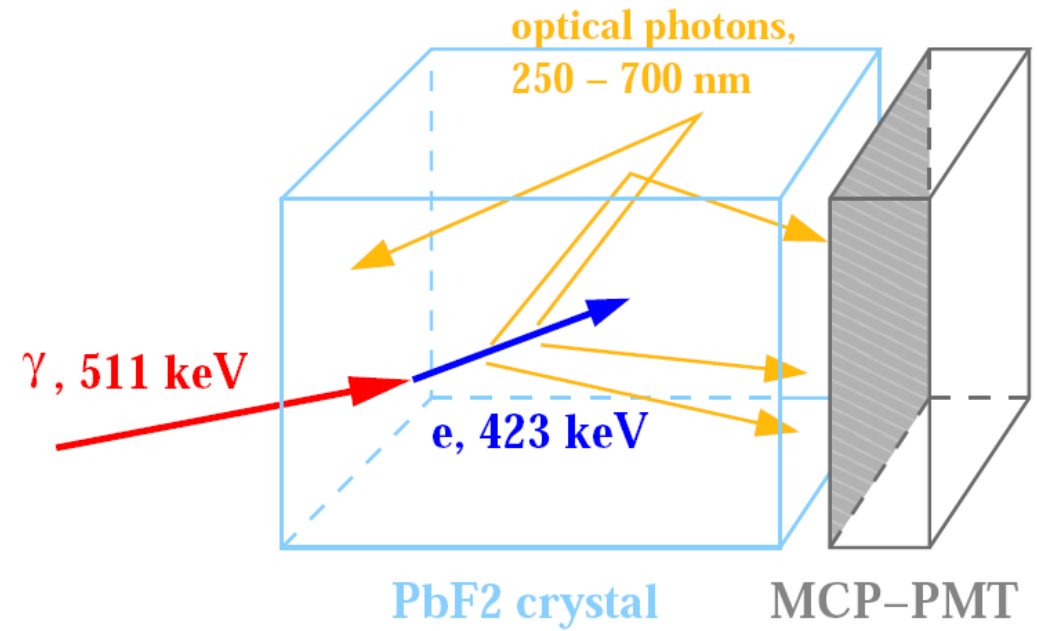
- TOF techniques: measure the difference in time between two photons  
⇒ improve S/B
- Contrast of the image directly correlated to the S/B and available statistics.
- TOF gain estimation:

$$G = \frac{S/N_{TOF}}{S/N_{noTOF}} \sim \sqrt{\frac{D}{\delta x}} \sim \sqrt{\frac{D}{c/2 \delta t}}$$

$D=30 \text{ cm} \Rightarrow \text{CRT}=\mathbf{150 \text{ ps}}$  (FWHM)  $\Rightarrow G\sim 2.9 \Rightarrow \mathbf{8x \text{ lower dose}}$

# Previous Studies: Cherenkov Detection

- **High resolution TOF and high efficiency** for whole-body PET : **PECHE** project
  - Non-scintillating crystal,  $\text{PbF}_2$ , as a detection medium
  - Use Cherenkov light for the detection  $\rightarrow$  Radiation time  $\sim$  few ps
  - Goal: CRT < 100 ps (FWHM)
  - Use the fastest type of PMT : micro-channel-plate PMT
  - Use the dedicated high-speed digitizing electronics developed by IRFU and LAL, IN2P3

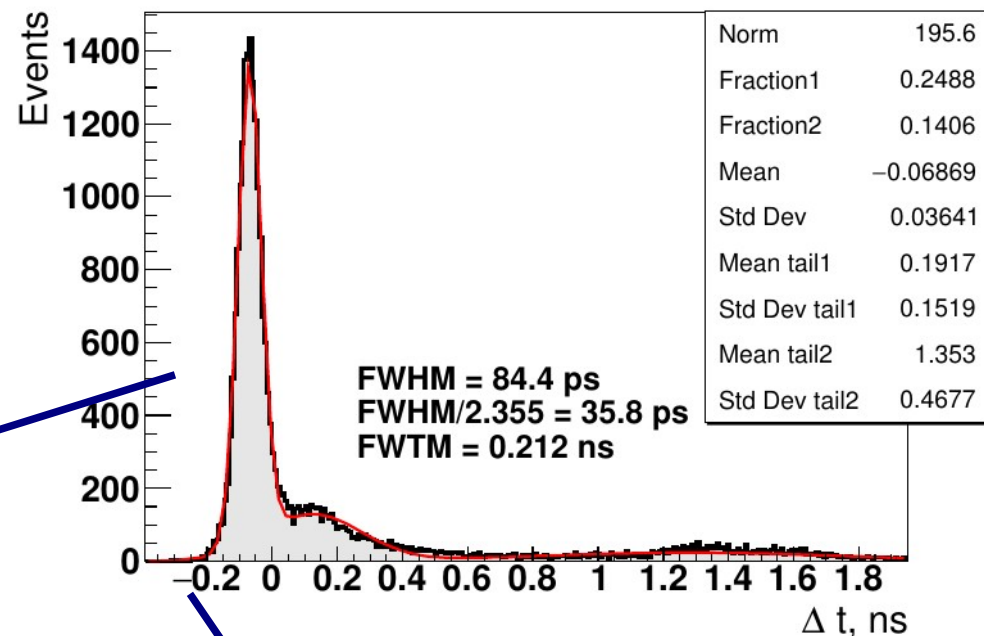


*C. Canot et al., J. Inst. 14 P12001 (2019) arXiv:1909.06107*

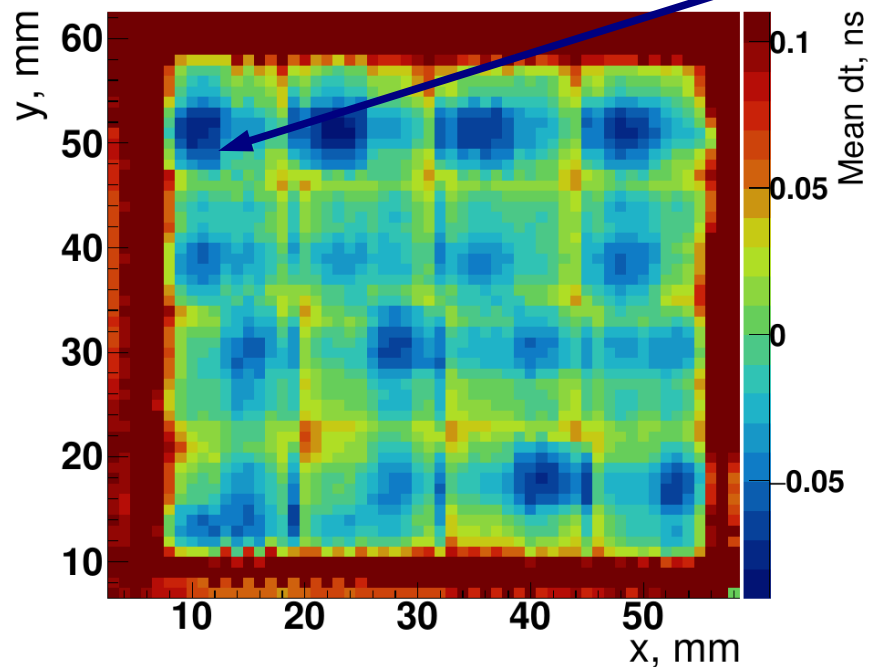


# Previous Studies: PMT Readout

- Measure time difference between PMT and pulse laser (20 ps beam duration)
- 1 mm step size
- ~70kHz acquisition speed
- ~2 hours per PMT

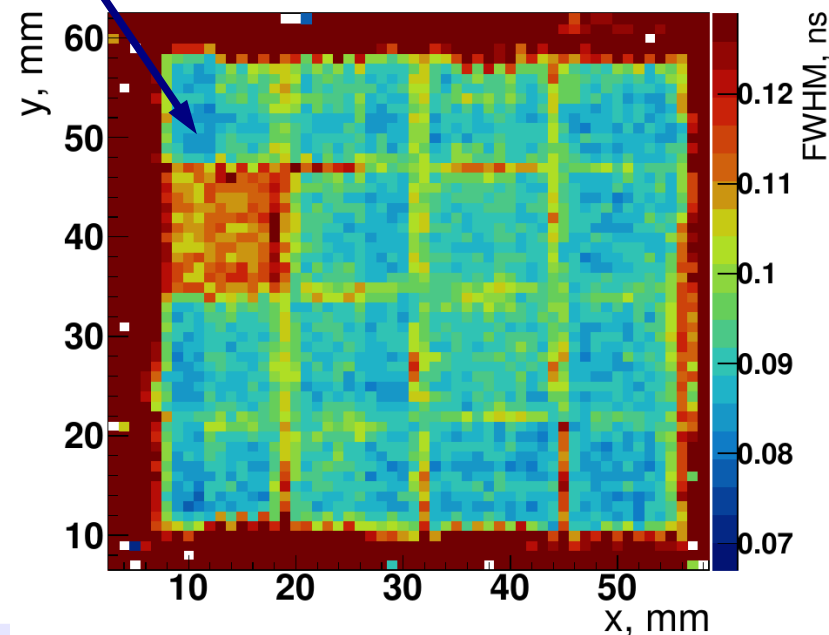


**Distribution Mean**

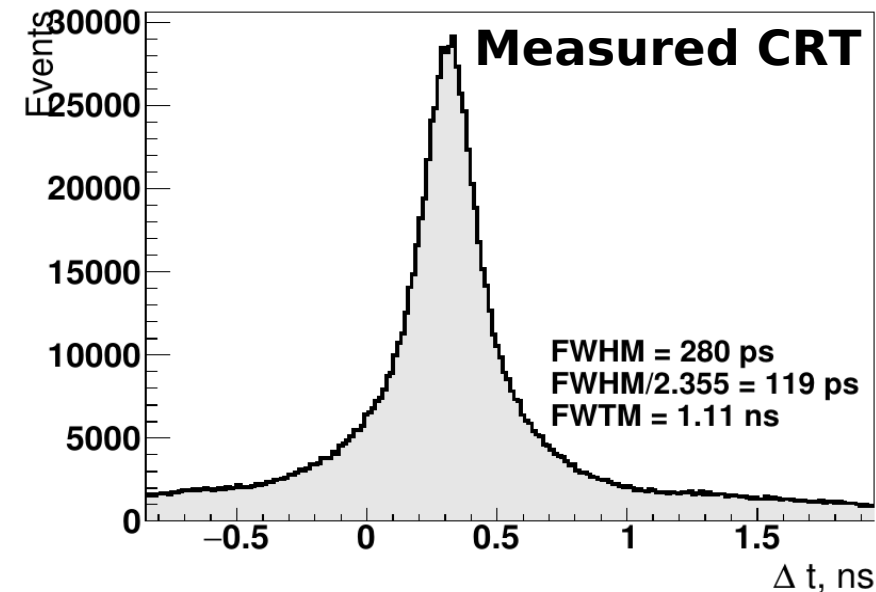
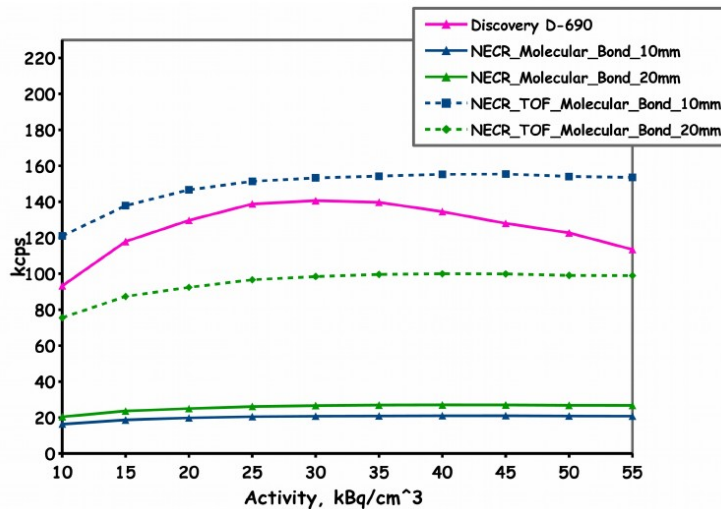
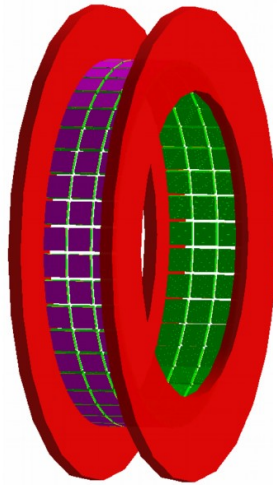


⇒ **Need to apply a time calibration as a function of (x,y)**

**Distribution Width**



# Previous Studies: Results



$$NECR = T^2 / (T + S + 2R)$$

$$NECR_{TOF} = D / \Delta x * NECR$$

T - rate of true coincidences  
 S - rate of scatter coincidences  
 R - rate of random coincidences

- Full chain of the high-efficient, large surface, Cherenkov based detection module : efficiency of ~**25%** and CRT of **280 ps** (PbF<sub>2</sub>)
- In the optimal-case scenario the Cherenkov whole body PET could be comparable with commercial devices: not very encouraging.
- To optimized CRT: (1) Increased number of the detected optical photons; (2) Continuous read-out in order to use the full potential of the PMT

M. Alokhina,  
 "Design of the Cherenkov TOF whole-body PET ..."  
 PhD thesis, 2018



# *ClearMind Project*

## *Efficient Cherenkov and Scintillation Detection With High Spatial Precision and high TOF for brain/whole body PET*

### ClearMind Collaboration :

- **CEA Saclay - DRF/IRFU**, D. Yvon, V. Sharyy, M. Follin, C-H. Sung, et al., (+ E. Delagne et al.), Patent accepted.
- **CNRS - IJC Labs - Orsay**, Service d'Electronique, D. Breton, J. Maalmi et al.
- **CNRS - IN2P3/CPPM - Marseille**, C. Morel, M. Dupont, et al.
- **CEA Saclay - DRF-ISVFJ/SHFJ** – S. Jan, C. Comtat, et al.
- **CEA Saclay - DES-ISAS/LGLS** – J.M. Martinez

### With :

#### Chemistry advices :

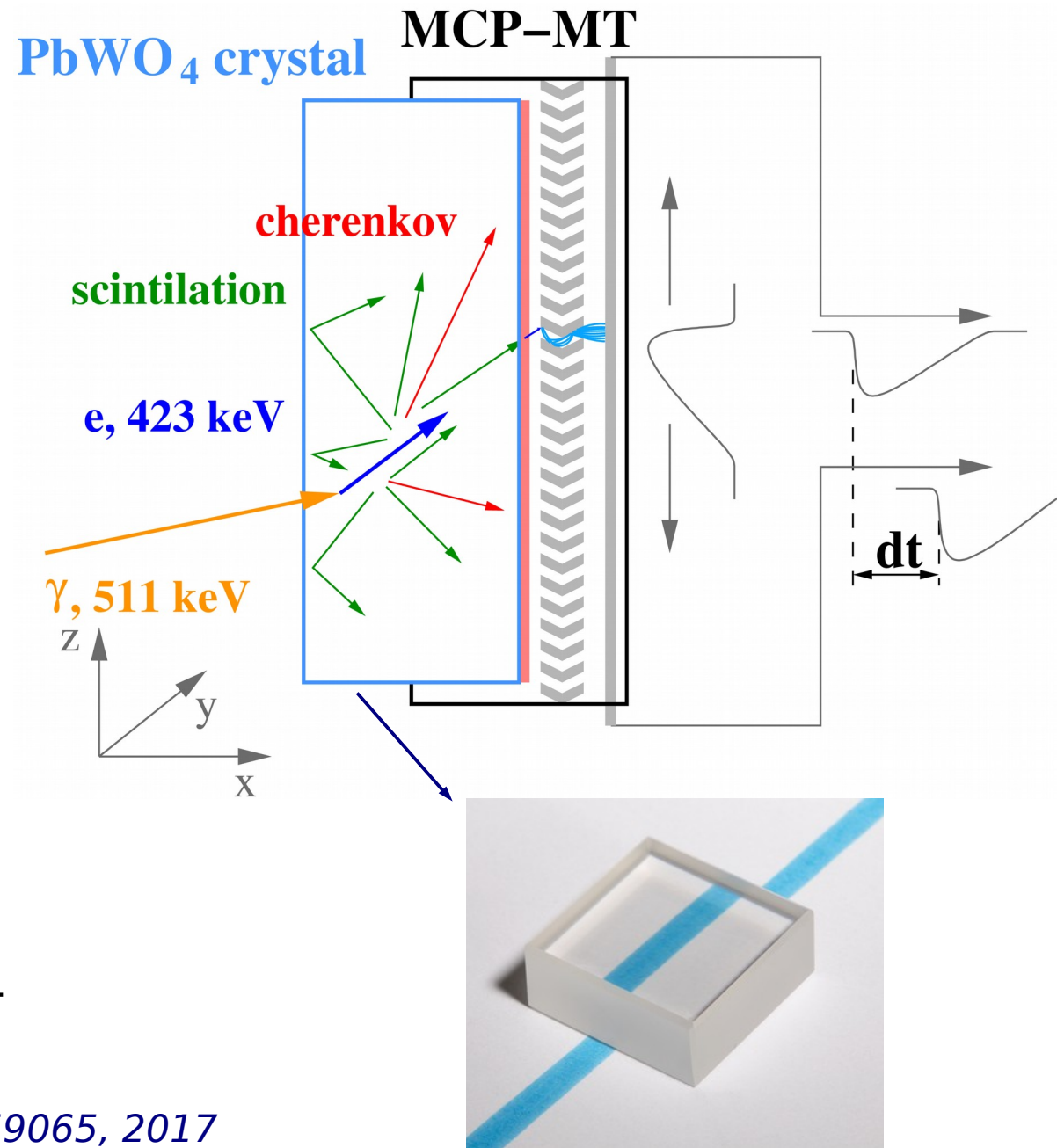
- **CEA-DRF/IRAMIS** – J-Ph. Renault, CEA-DEN/DPC/SCP – S. Chatain, CEA-DEN

#### Scintillating Crystals :

- **Belarusian State University**, Research Inst. for Nuclear Problems- M. Korjik.

# Principles

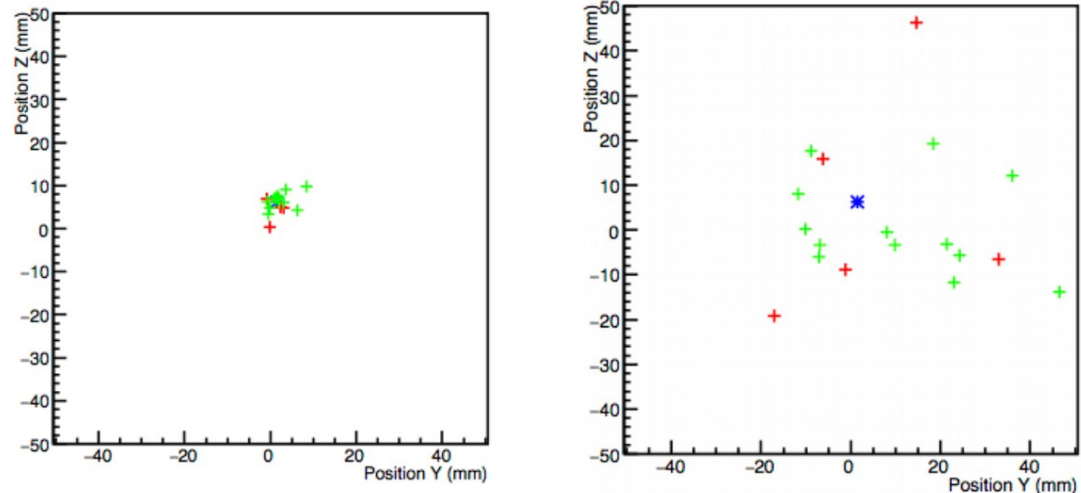
- Direct deposition of the photocathode on the  $\text{PbWO}_4$  crystal: “**scintronic**” crystal
  - increase the number of detected Cherenkov photons
  - additional fast scintillation photons
- Use of monolithic crystal to reconstruct 3D interaction position and correct for DOI effect
- Use MCP for electron multiplication
- Use transmission line approach to reduce number of channels and improve PMT calibration



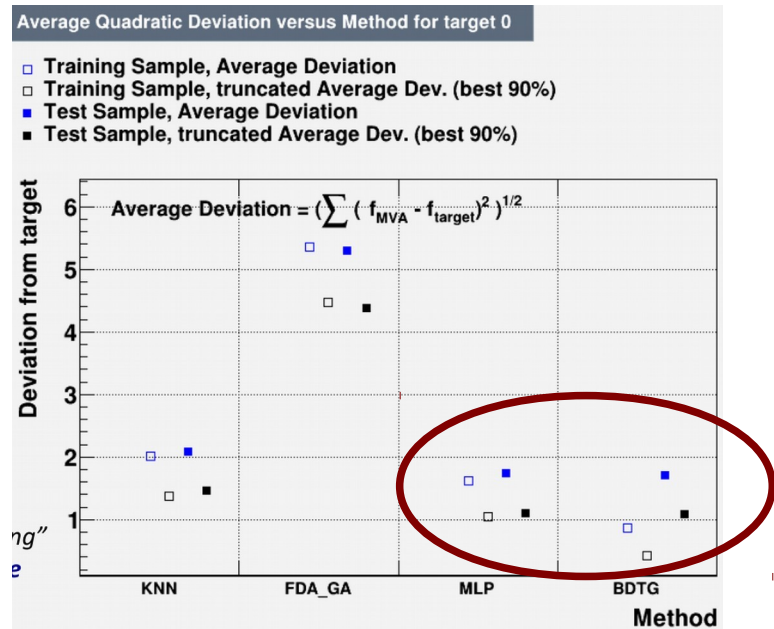
Patent CEA, FR1759065, 2017

# ClearMind: expected performances

- Allow to increase by a factor of  $\sim 4$ , the number of generated photo-electrons
- Has a potential to reconstruct both all three coordinates inside the crystal with the precision of 1 - 2 mm.
  - The machine learning approach is needed to reach the optimal performance
- Time resolution: corrected for the DOI  $\rightarrow$  expected CRT below 100~ps

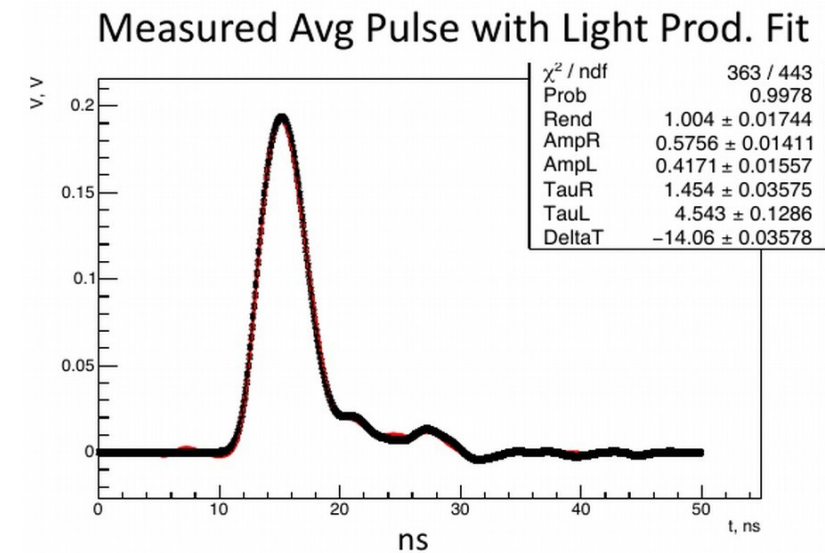
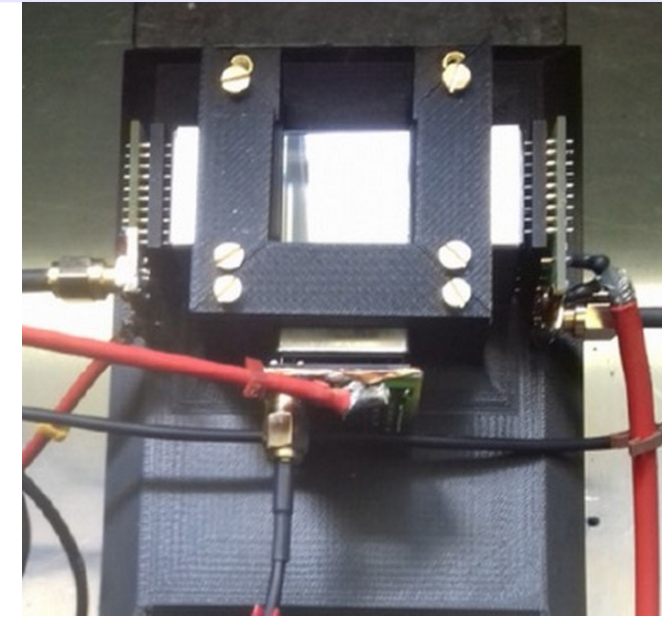


## Machine Learning Approach



# Crystal Performance

- Four PbWO<sub>4</sub> technologies available:
  - CRYTUR: Panda II.
  - SICCAS : CMS
  - SICCAS: Yttrium-doped
  - EPIC: Undoped PbWO<sub>4</sub>
- Monté-Carlo simulation (GATE-GEANT4)
- Light-Yields Measurements: all doped crystals show similar light yields  $\sim 10\%$  : 300  $\gamma$ /MeV
- Scintillation time constant: short  $\sim 1.5$  ns, slow  $\sim 5$  ns @ 20°C
- Undoped crystal shows an additional very slow component.
- Large size Crystals are produced by Crytur

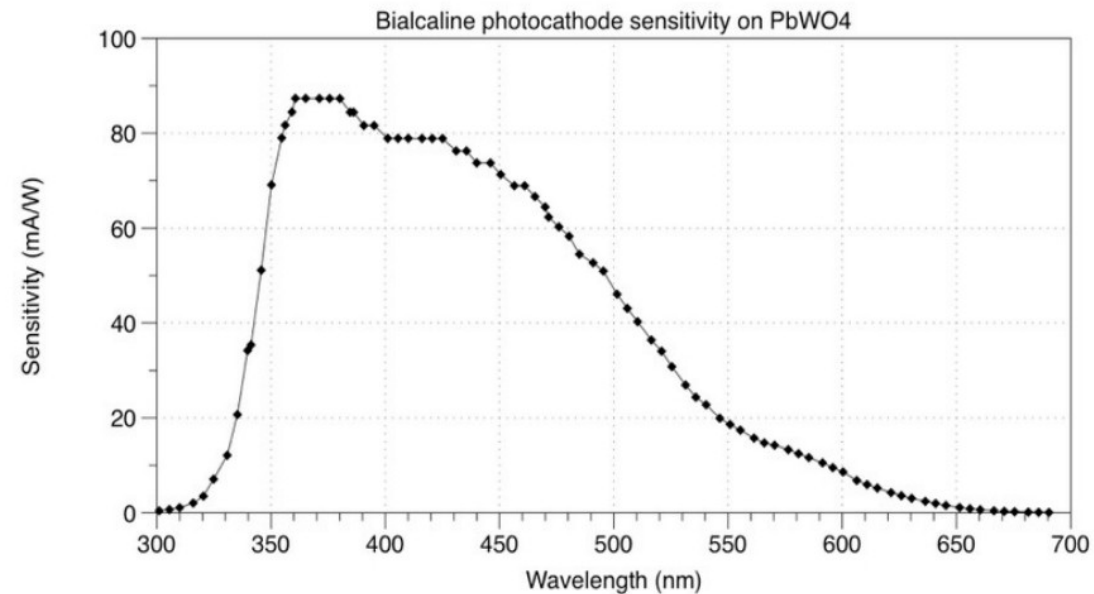
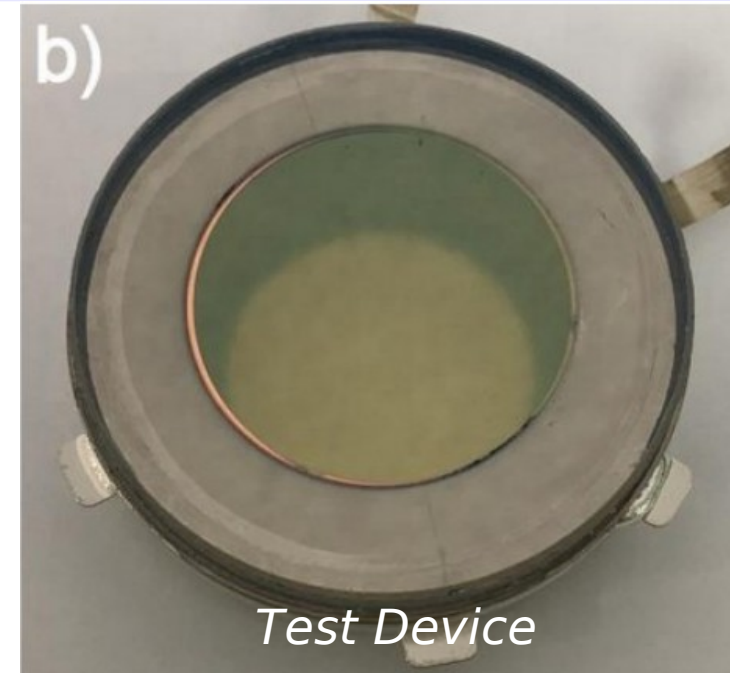


To be published soon: *M. Follin et al., JINST*

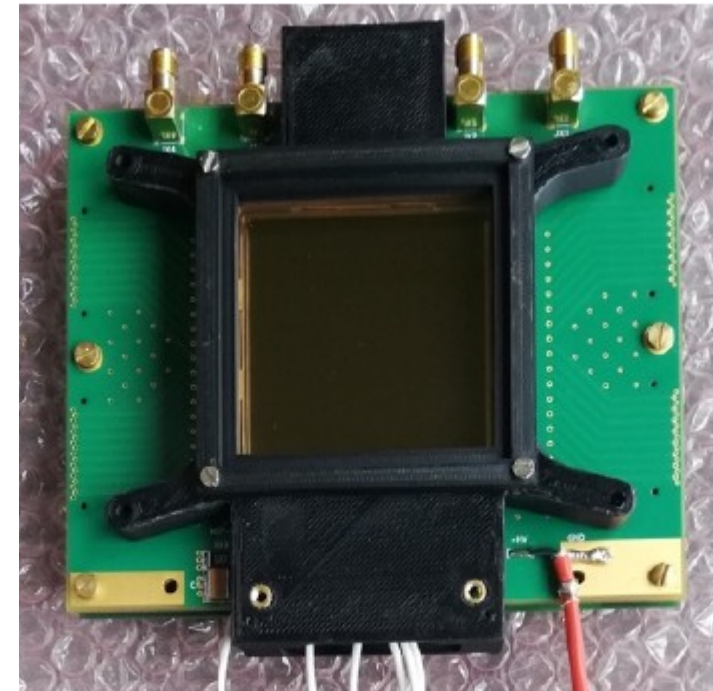
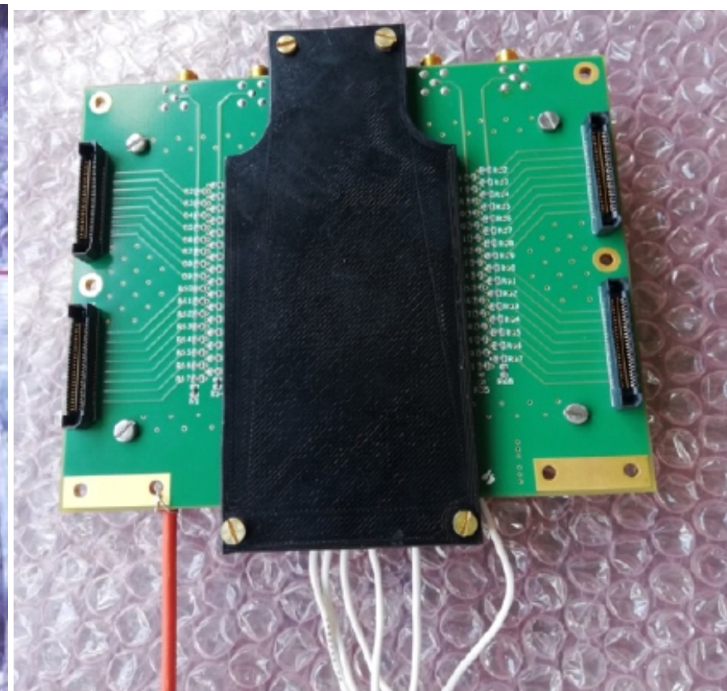
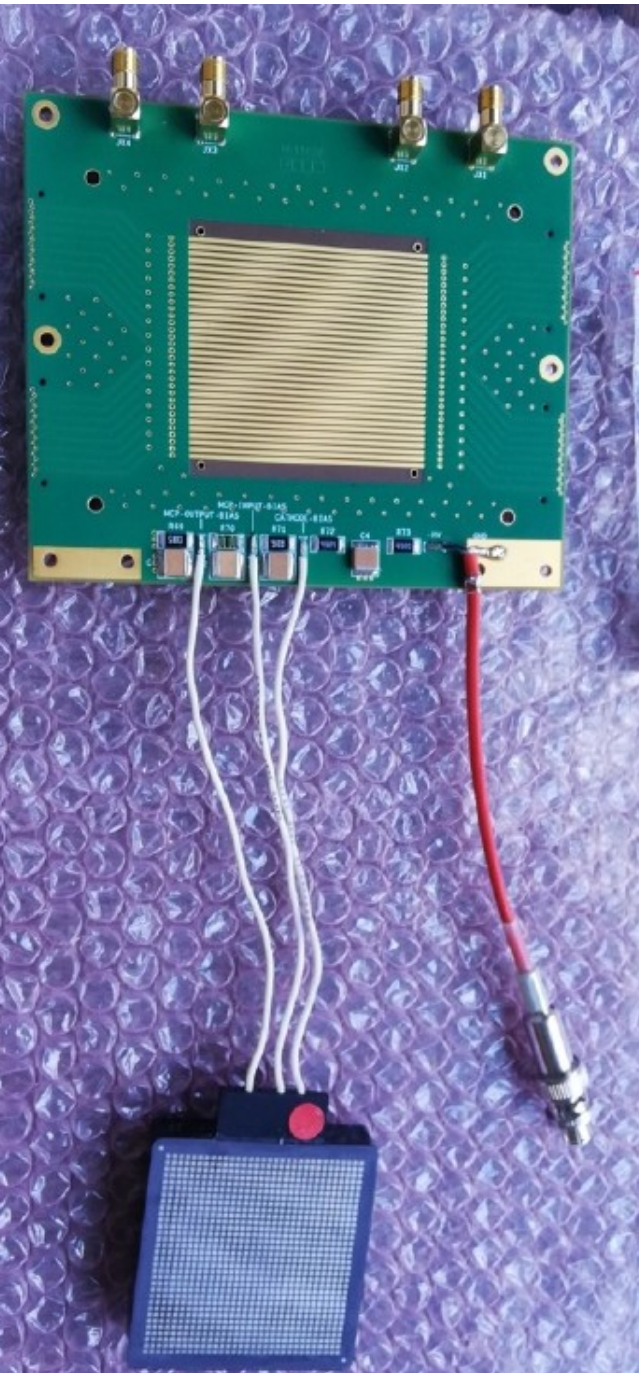


# PhotoCathode Deposition Tests

- R&D with Photek, UK
- Crystal produce by CRYTUR, Czech Republic
- Final test device:
  - 25% peak efficiency
  - Stable over 9 months
  - Still can be improved
  
- **Major milestone achieved!**



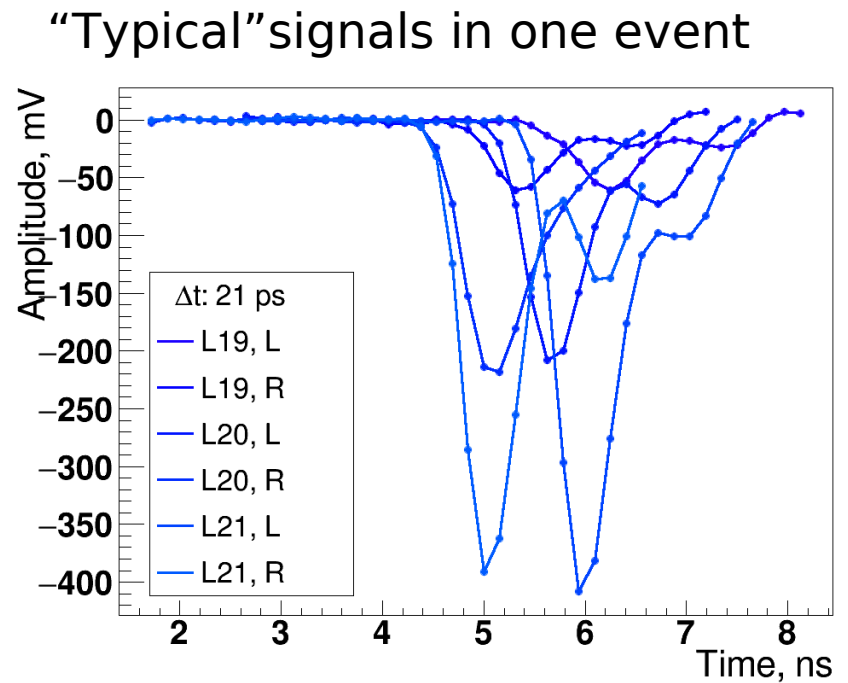
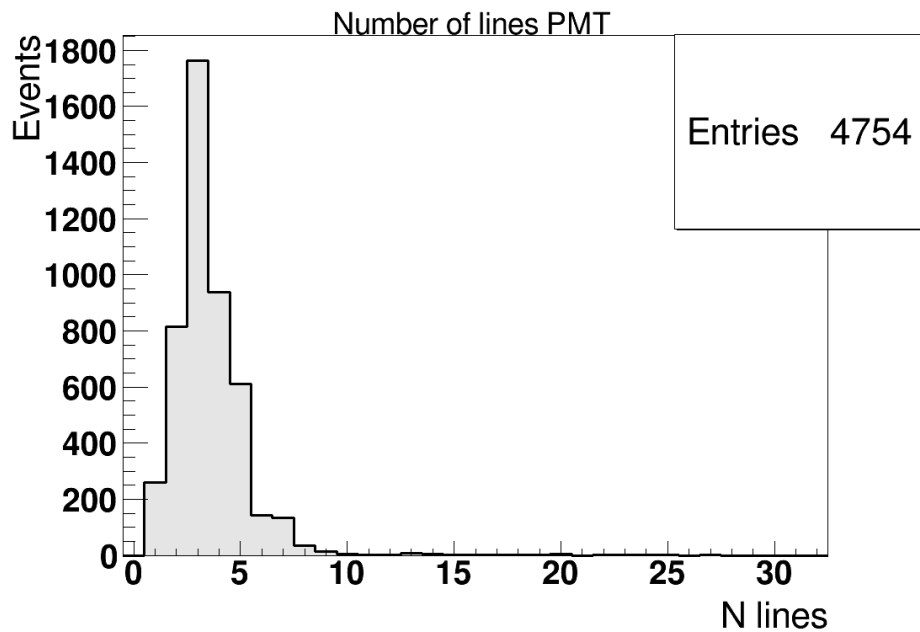
# Transmission Line Readout





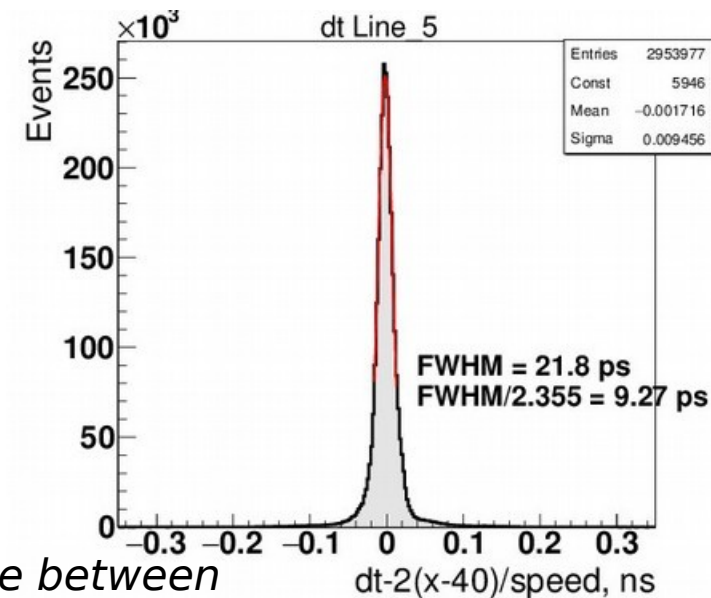
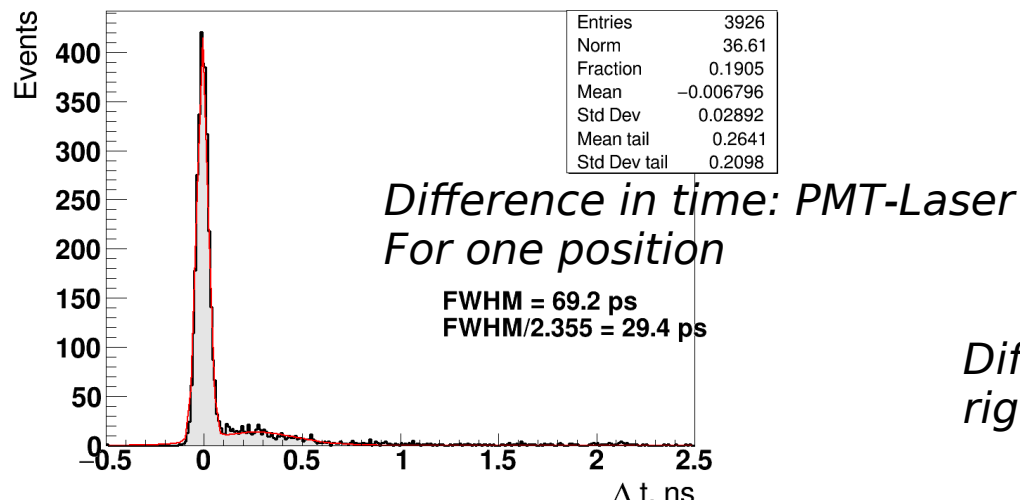
# Read-out Through the Transmission Lines

- Use 10  $\mu\text{m}$  Planacon MCP-PMT, 32x32 pads, 1.6 mm pitch
- Read-out with 32 transmission lines PCB.
- Both ends read-out through 40 db, 700 MHz LAL-made amplifiers and SAMPIC digitization module
- Using 20 ps pulsed laser to scan PMT

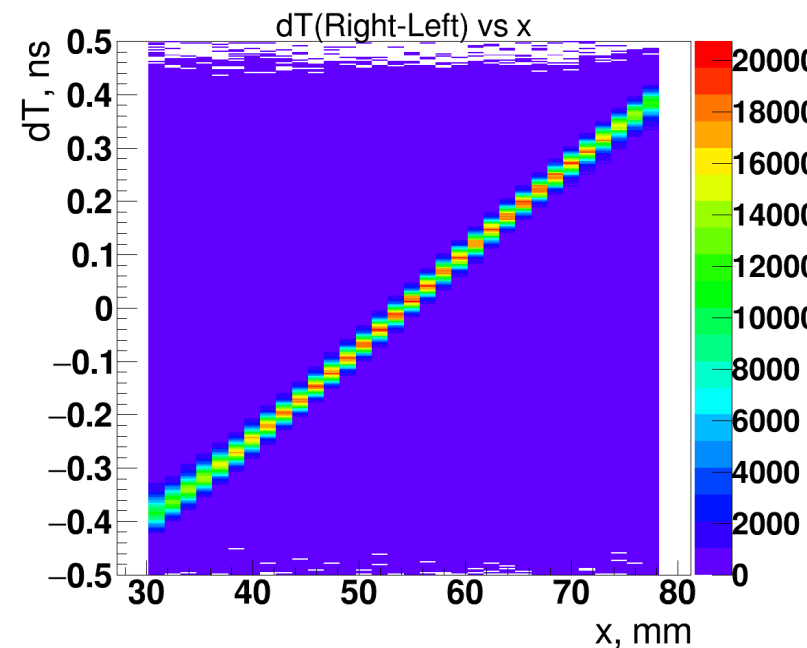
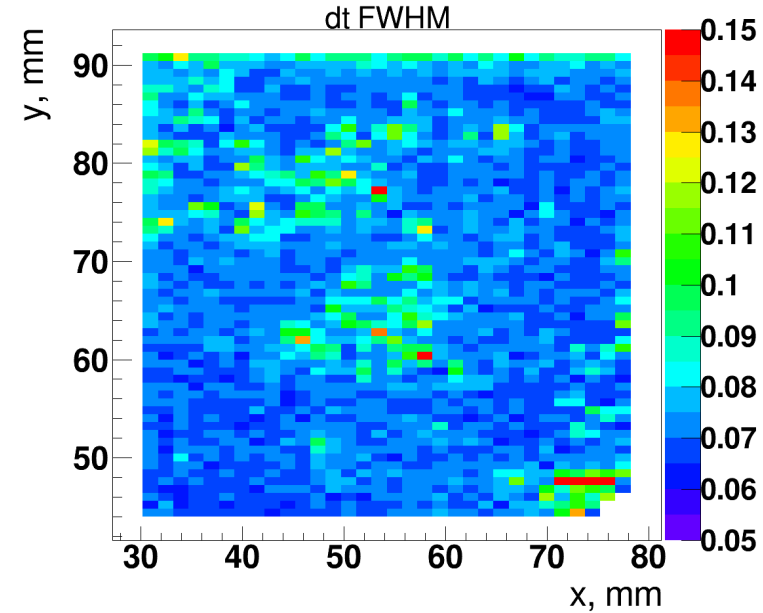


# Read-out Through the Transmission Lines

- Reach a  $\sim$  **20 ps** precision on time difference  
 $\rightarrow$  spatial resolution  $\sim$  **1 mm (FWHM)**
- Measured PMT TTS down to **70 ps (FWHM)**



Difference in time between right and left ends for one position



# Conclusion

- Development of the cutting-edge technology for use in PET, but not only.
- Main directions: high spatial precision and high TOF resolution
- Study a potential of the Cherenkov radiation for whole-body PET scanner by simulation and hardware test and identified main limitations for use of the Cherenkov technology
- The ongoing developments at IRFU have the ambition to overtake the identified limitations.
  - PET TOF high efficiency detection module with the 3D spatial resolution of **1-2 mm** and CRT < **100 ps**
- We are expecting to receive the 1<sup>st</sup> prototype before Christmas

